



(12) **United States Patent**
Burger et al.

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(54) **REPLACEABLE AND/OR EASILY
REMOVABLE NEEDLE SYSTEMS FOR
DERMAL AND TRANSDERMAL CRYOGENIC
REMODELING**

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patent is extended or adjusted under 35
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(51) **Int. Cl.**
A61B 17/56 (2006.01)
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CPC **A61B 18/0218** (2013.01); **A61B 18/02**
(2013.01); **A61B 2017/00747** (2013.01);
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(58) **Field of Classification Search**
CPC A61M 35/00; A61M 37/00; A61K 8/30;
A61K 8/33; A61B 18/02; A61B 18/08
USPC 606/20–25, 34; 600/439, 459
See application file for complete search history.

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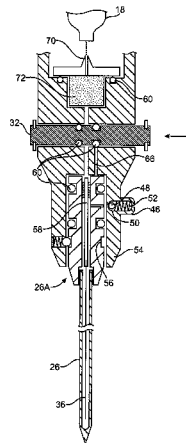
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(57) **ABSTRACT**

The present invention generally provides improved medical devices, systems, and methods. Some embodiments of the present invention apply cooling with at least one small, tissue-penetrating probe, the probe often comprising a needle having a size suitable for inserting through an exposed surface of the skin of a patient without leaving a visible scar. The cooling may remodel one or more target tissue so as to effect a desired change in a composition of the target tissue and/or a change in its behavior. Exemplary embodiments make use of replaceable needle probes supported by a probe body handle, with small needle probes often being replaced during treatment of a single patient. Careful control over the control of cryogenic cooling fluid into a needle probe can allow the length of the active cooling to be controlled through depletion of liquid from an evaporating cryogenic cooling flow.

23 Claims, 17 Drawing Sheets



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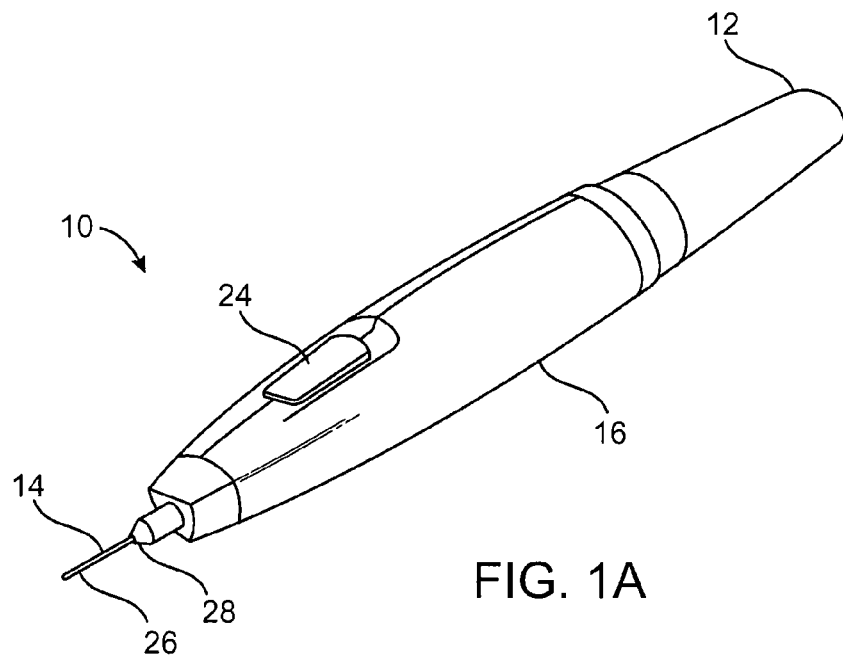


FIG. 1A

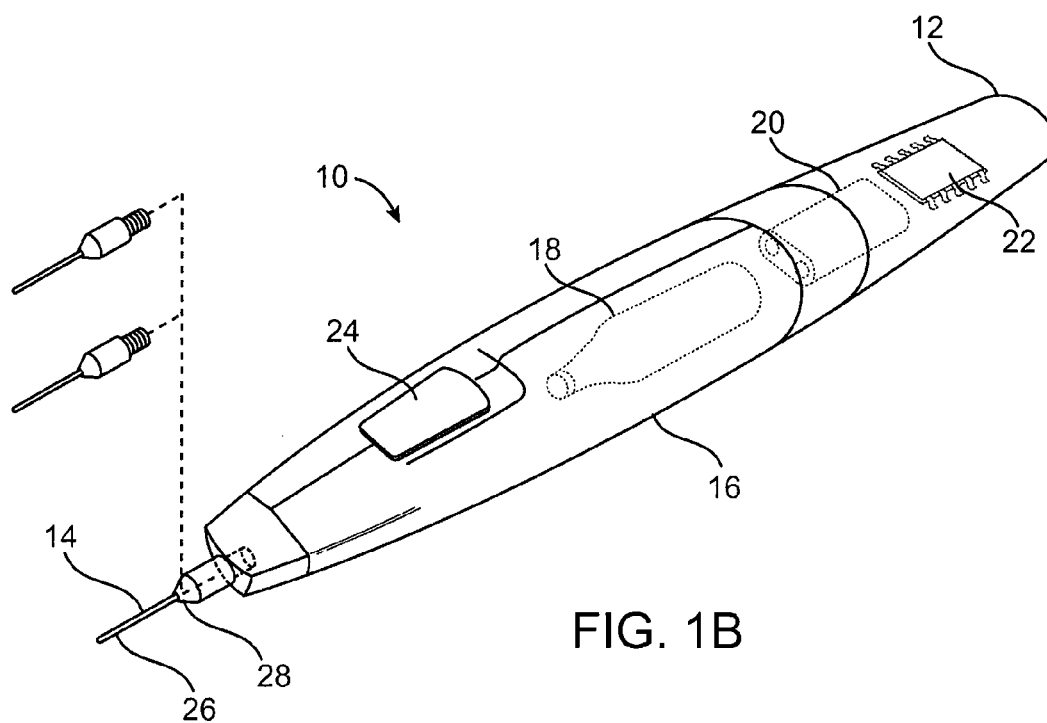
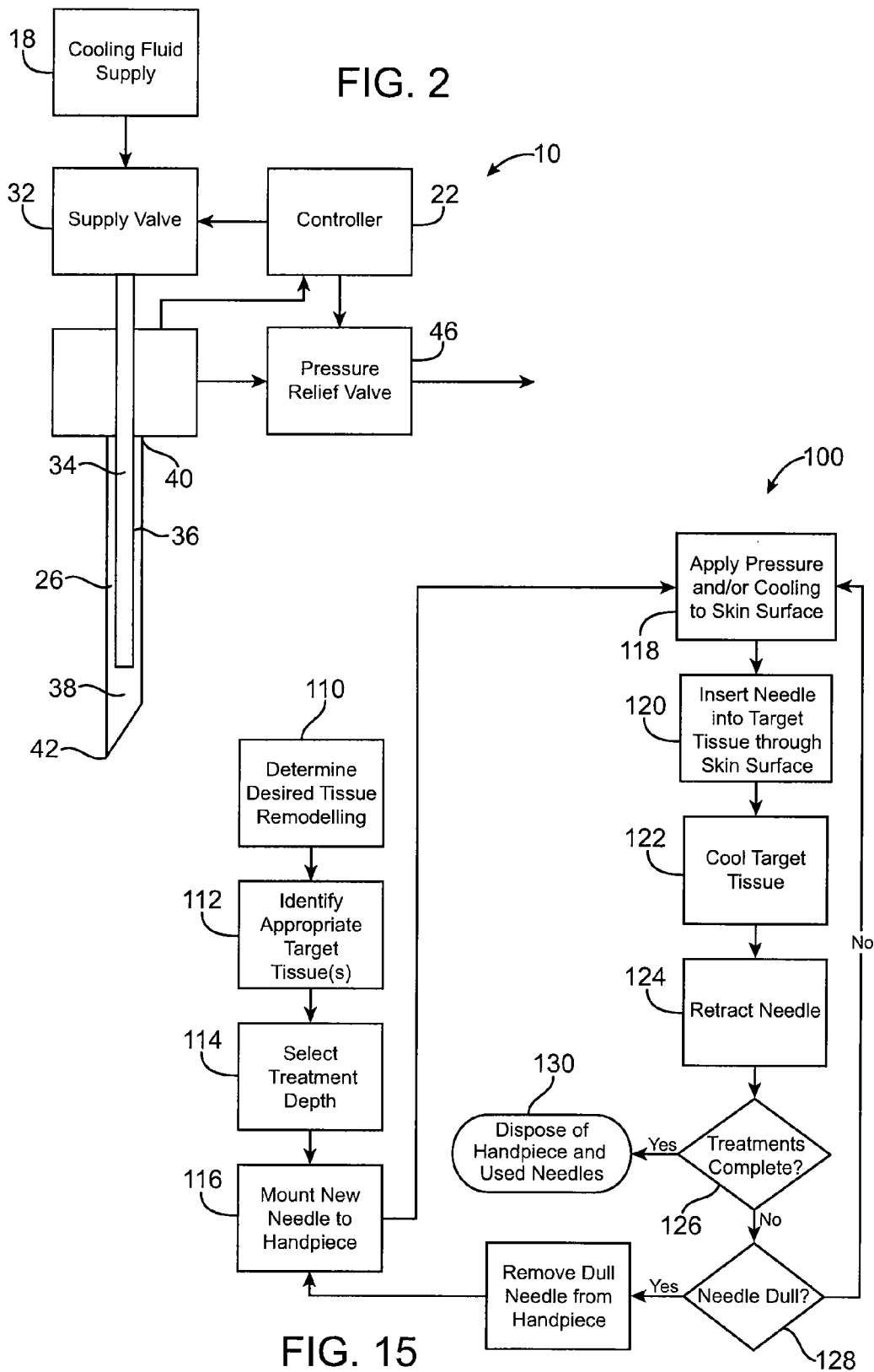


FIG. 1B



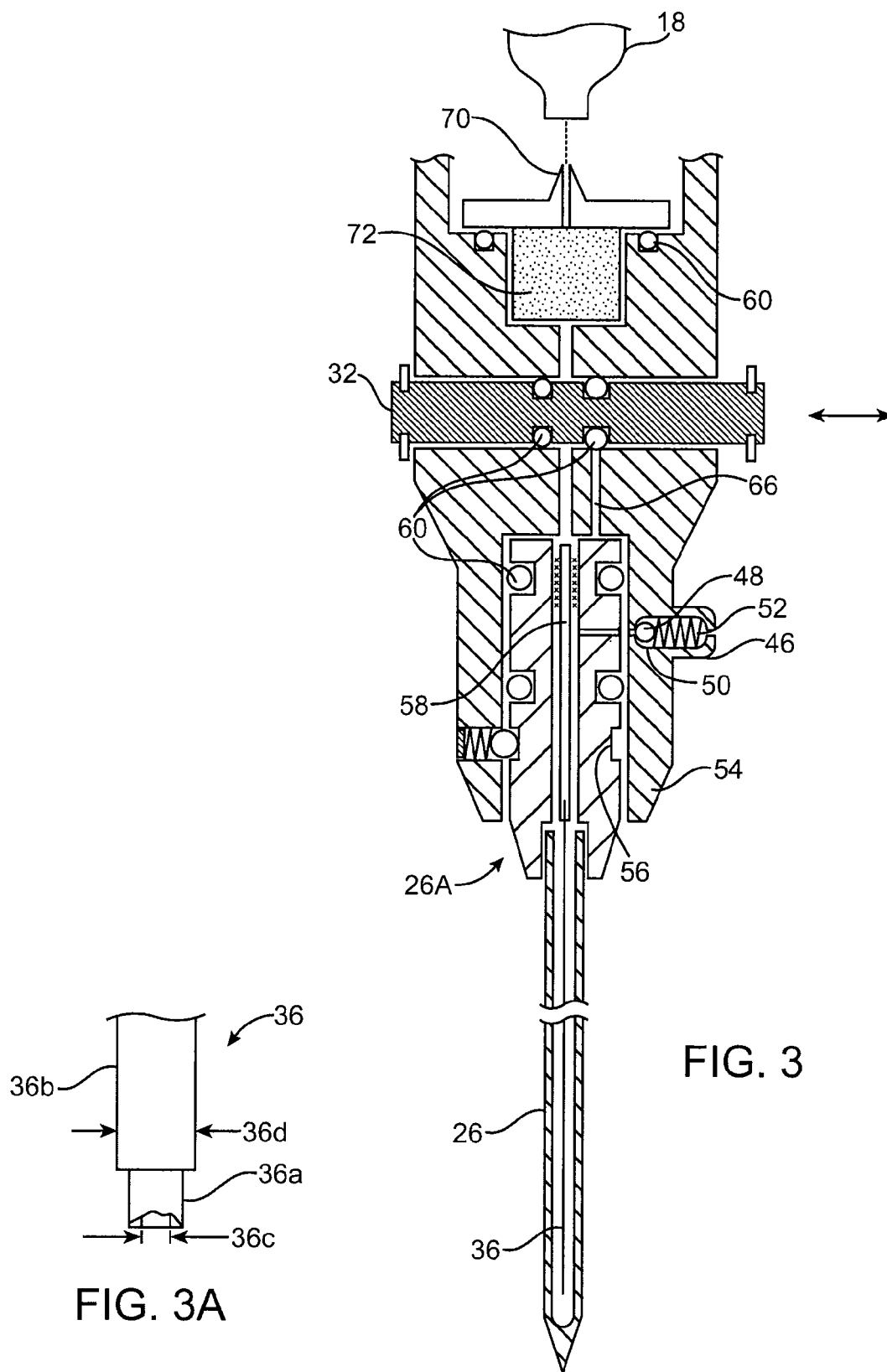


FIG. 3

FIG. 3A

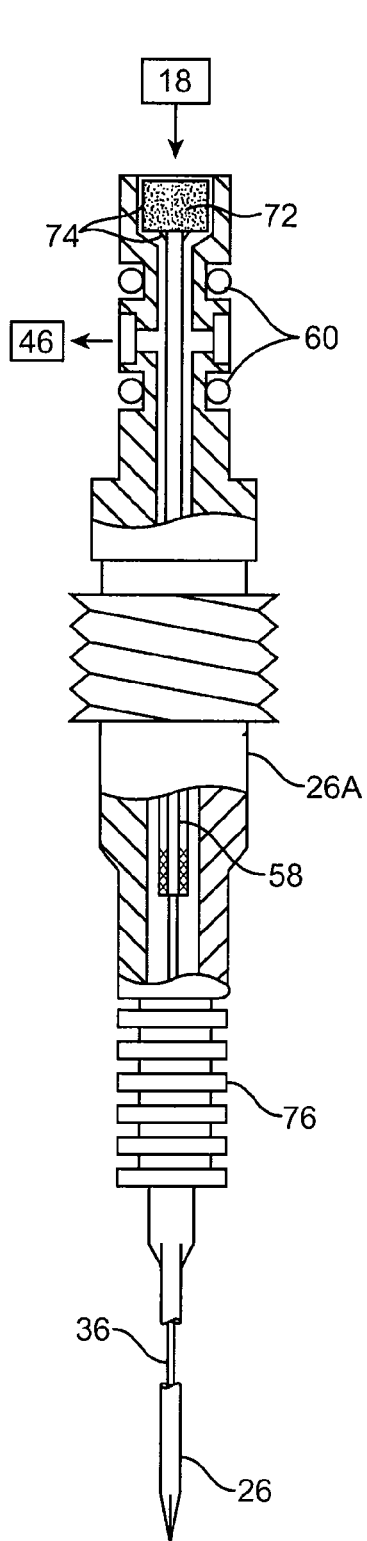


FIG. 4

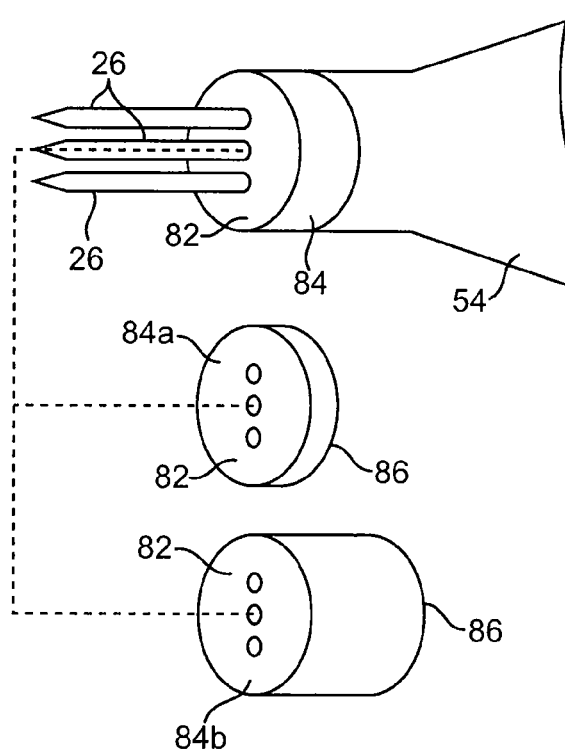


FIG. 6

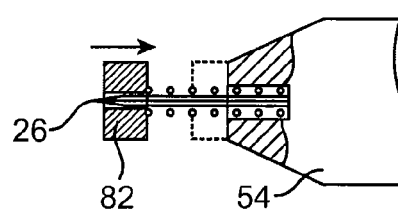


FIG. 7

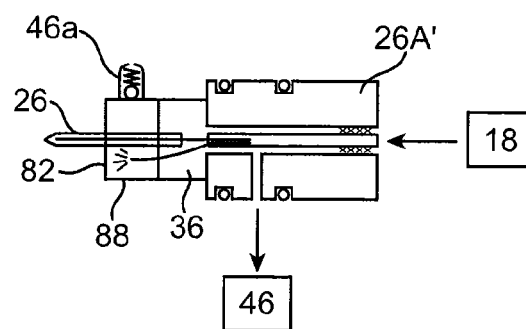


FIG. 8

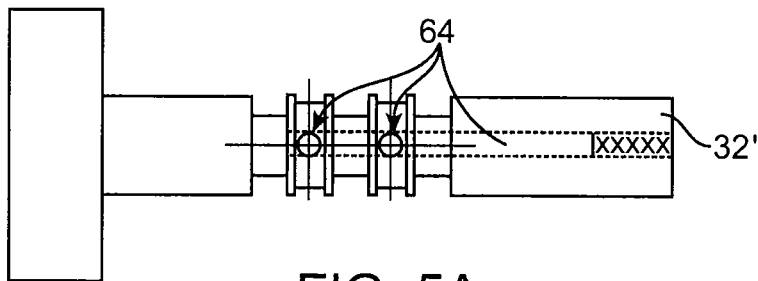


FIG. 5A

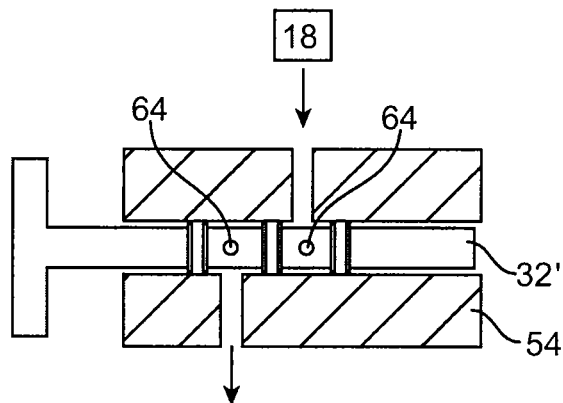


FIG. 5B

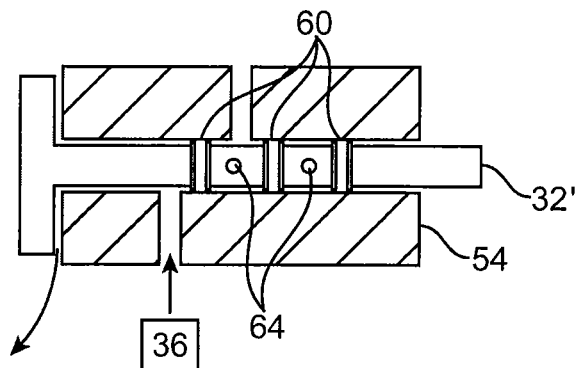


FIG. 5C

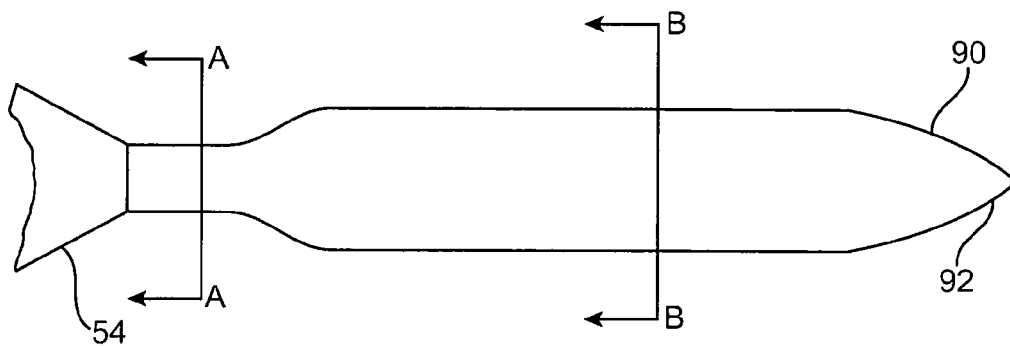
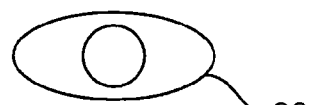


FIG. 9



Section
AA

FIG. 9A



Section
BB

FIG. 9B

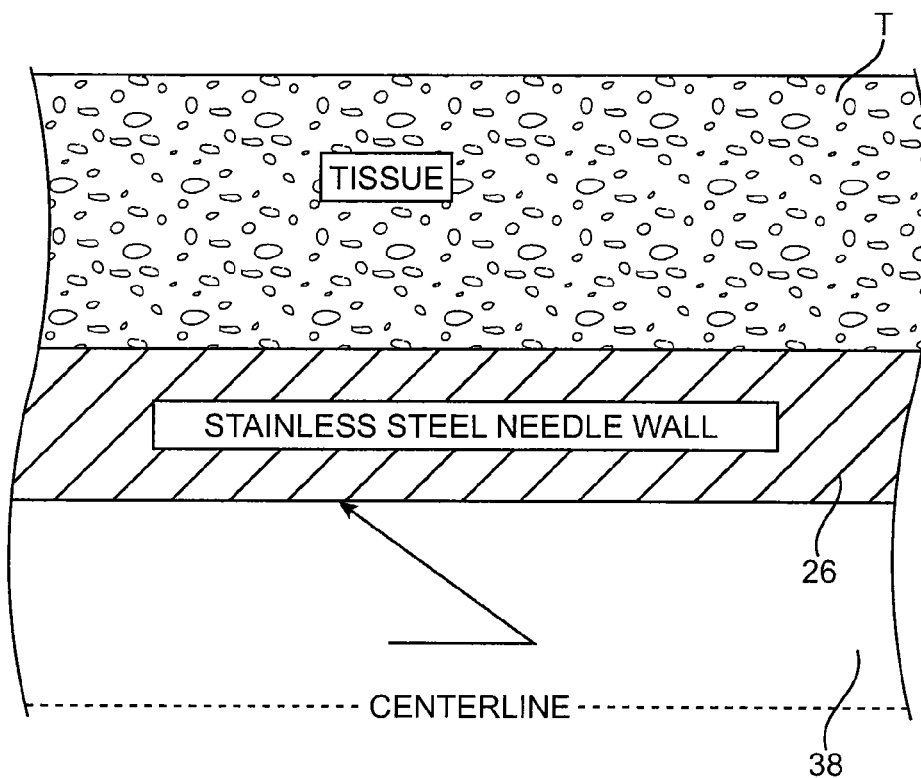


FIG. 10

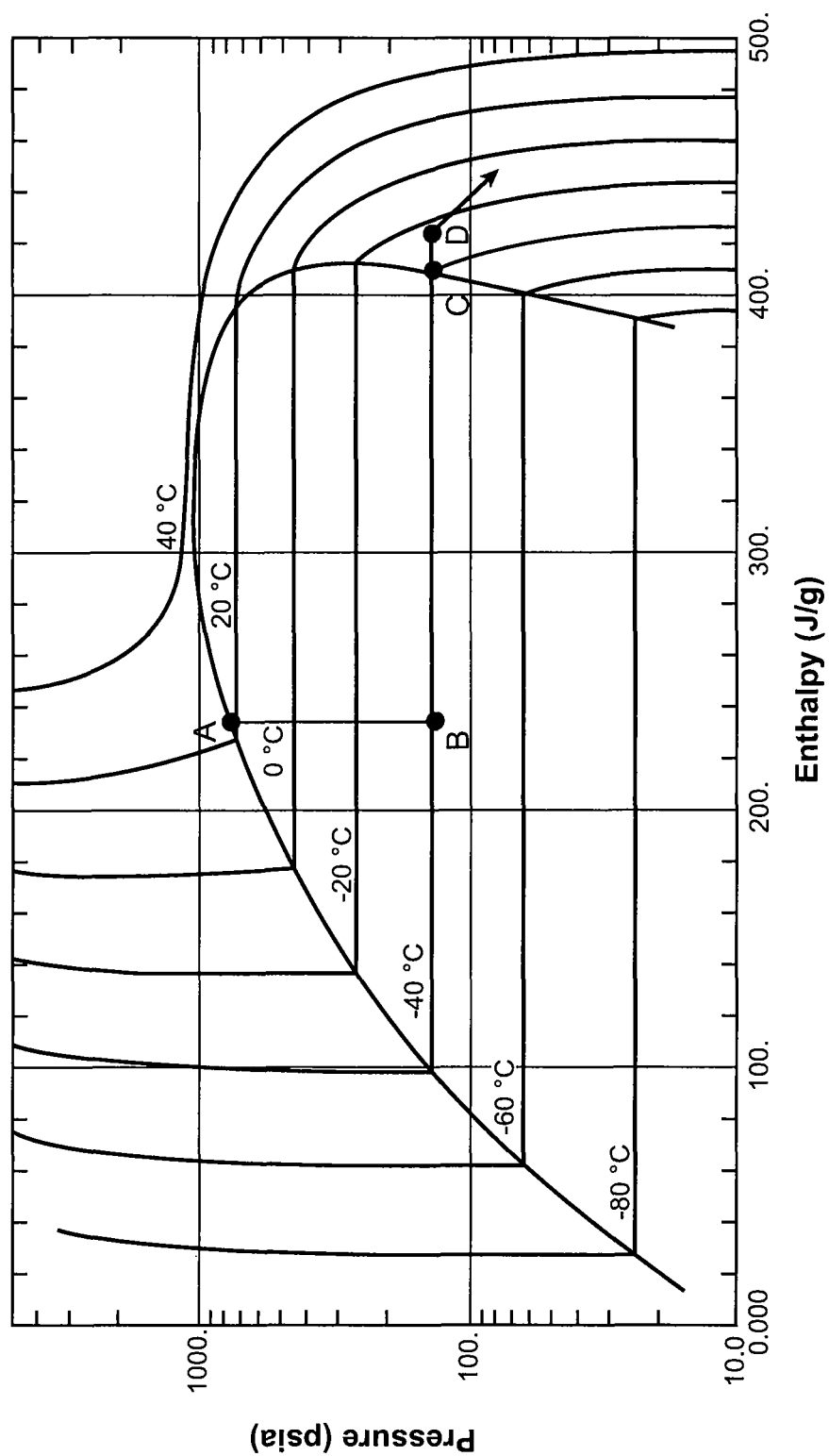


FIG. 10A

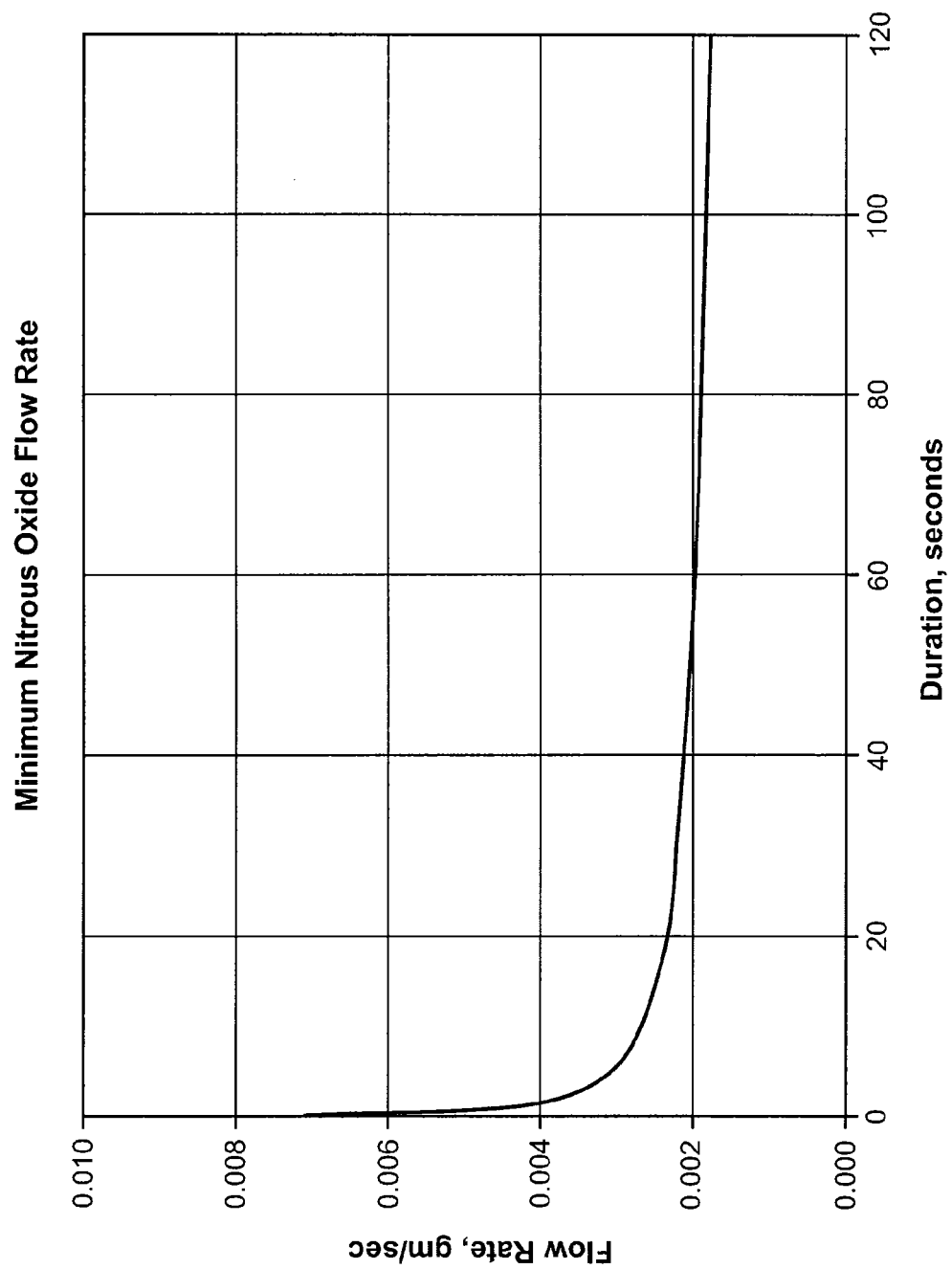


FIG. 10B

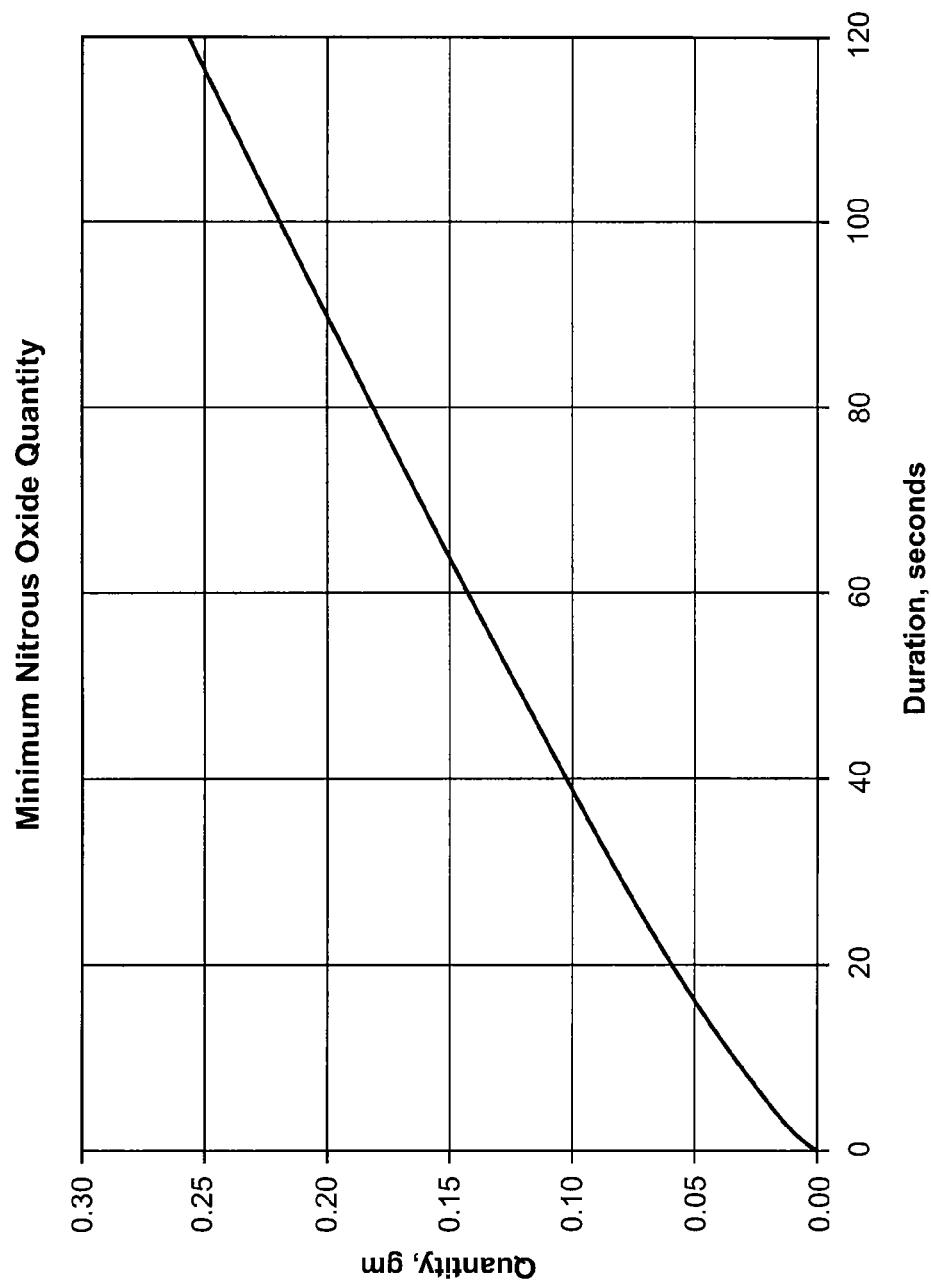


FIG. 10C

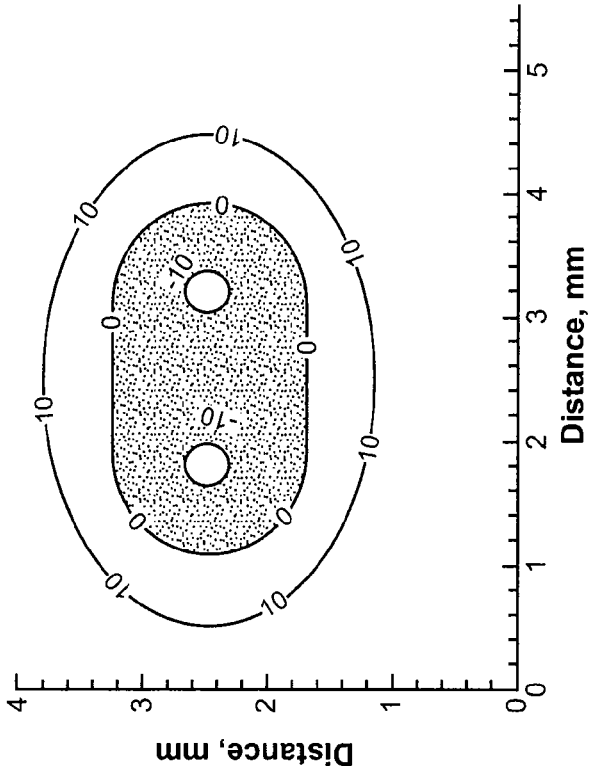


FIG. 11A

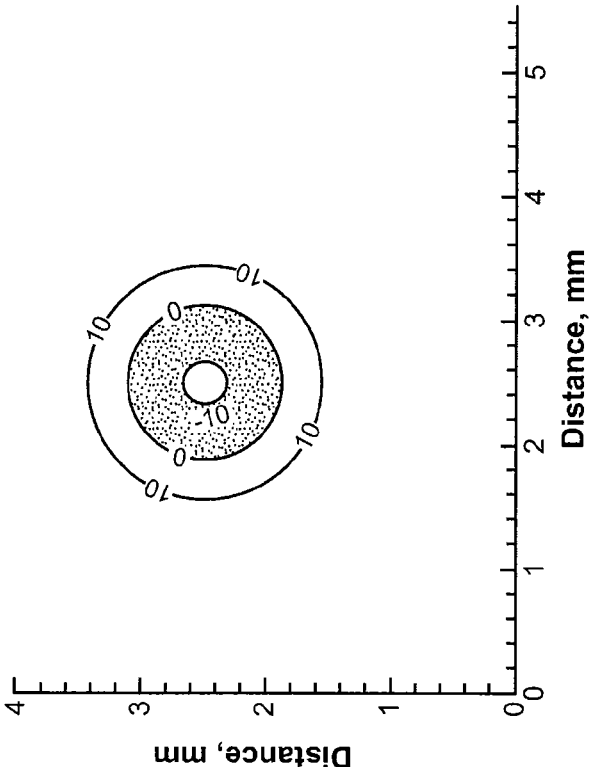


FIG. 11B

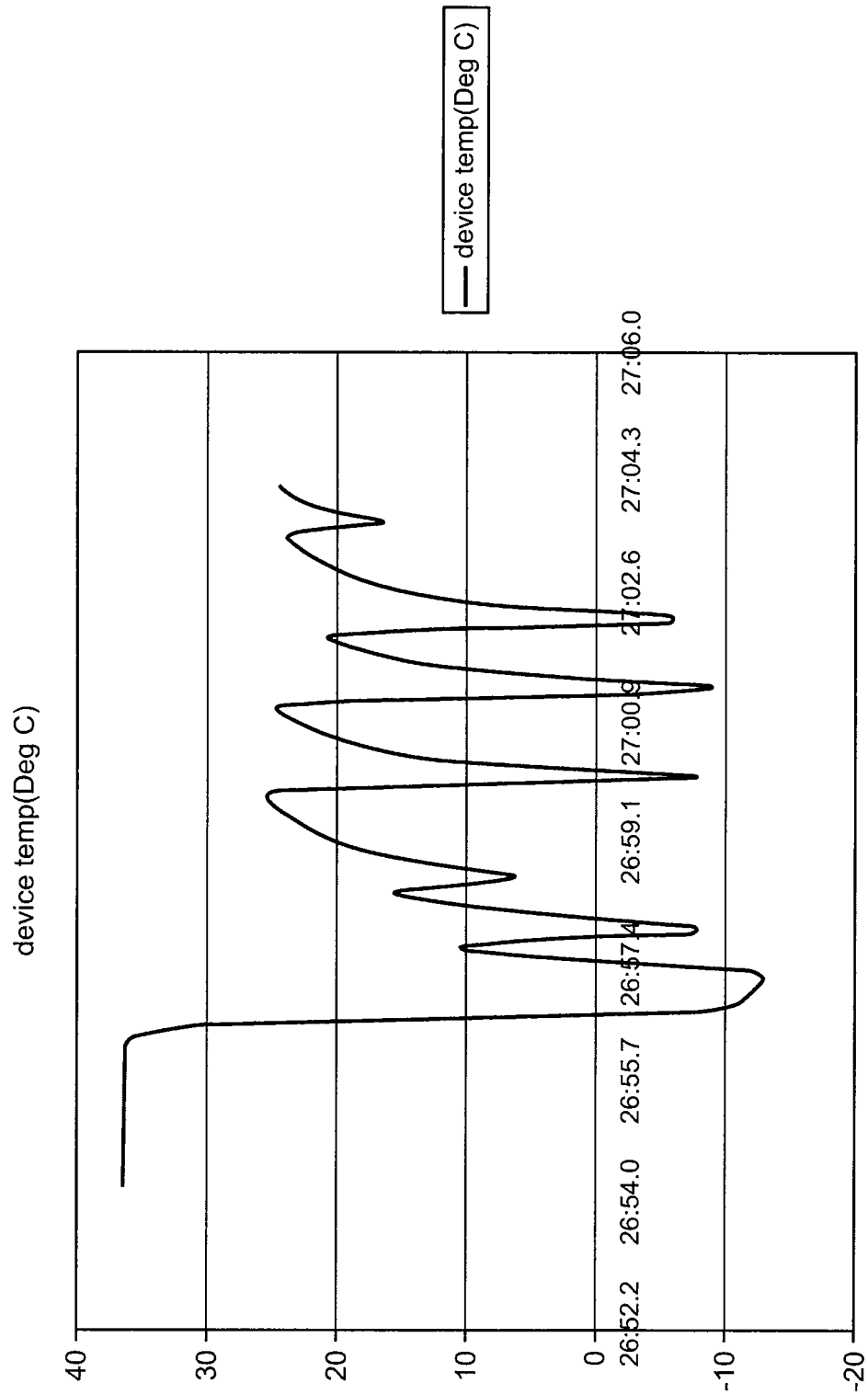


FIG. 12

Large Volume Exhaust greater than .009 cubic inches

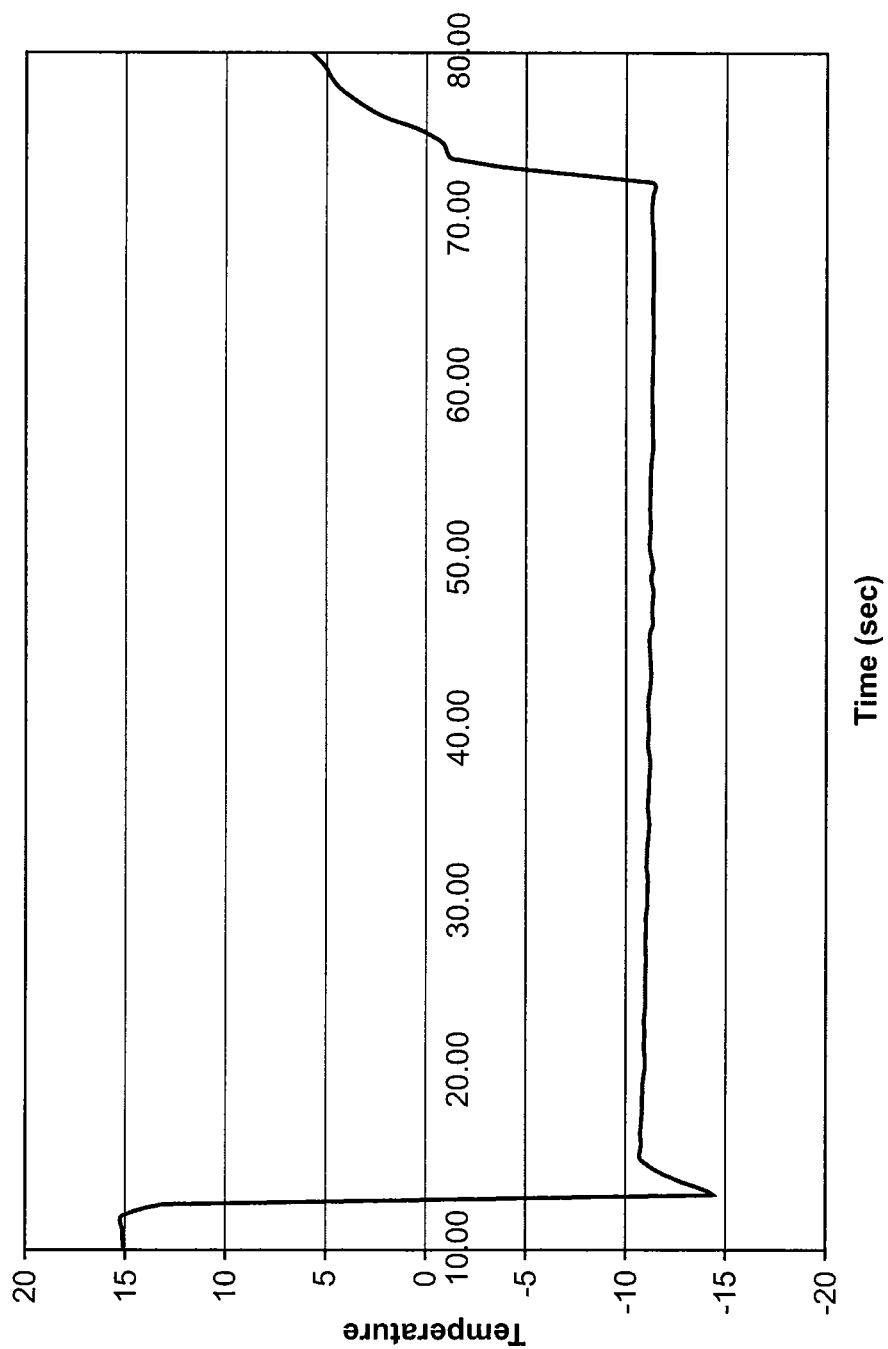


FIG. 13A

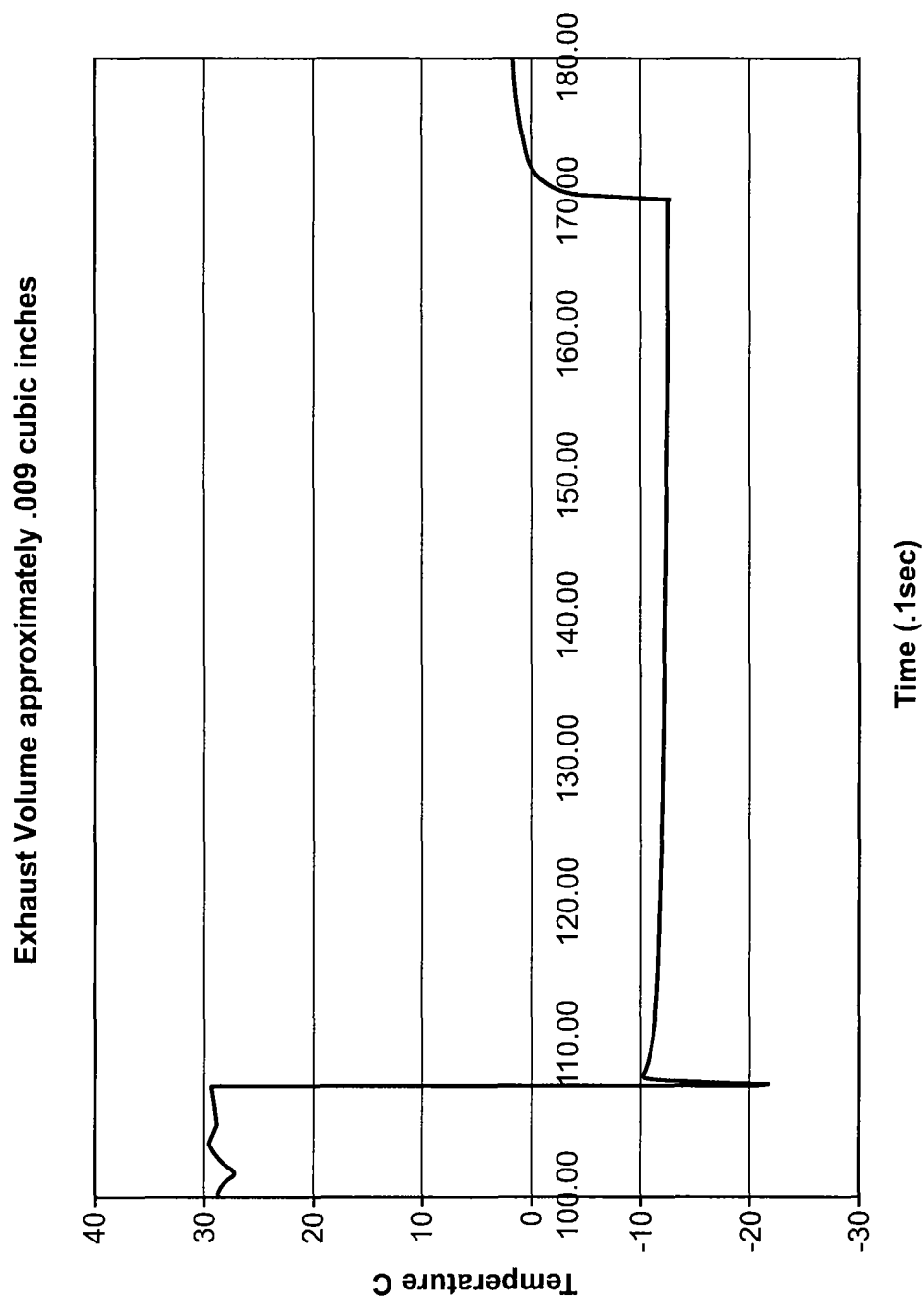


FIG. 13B

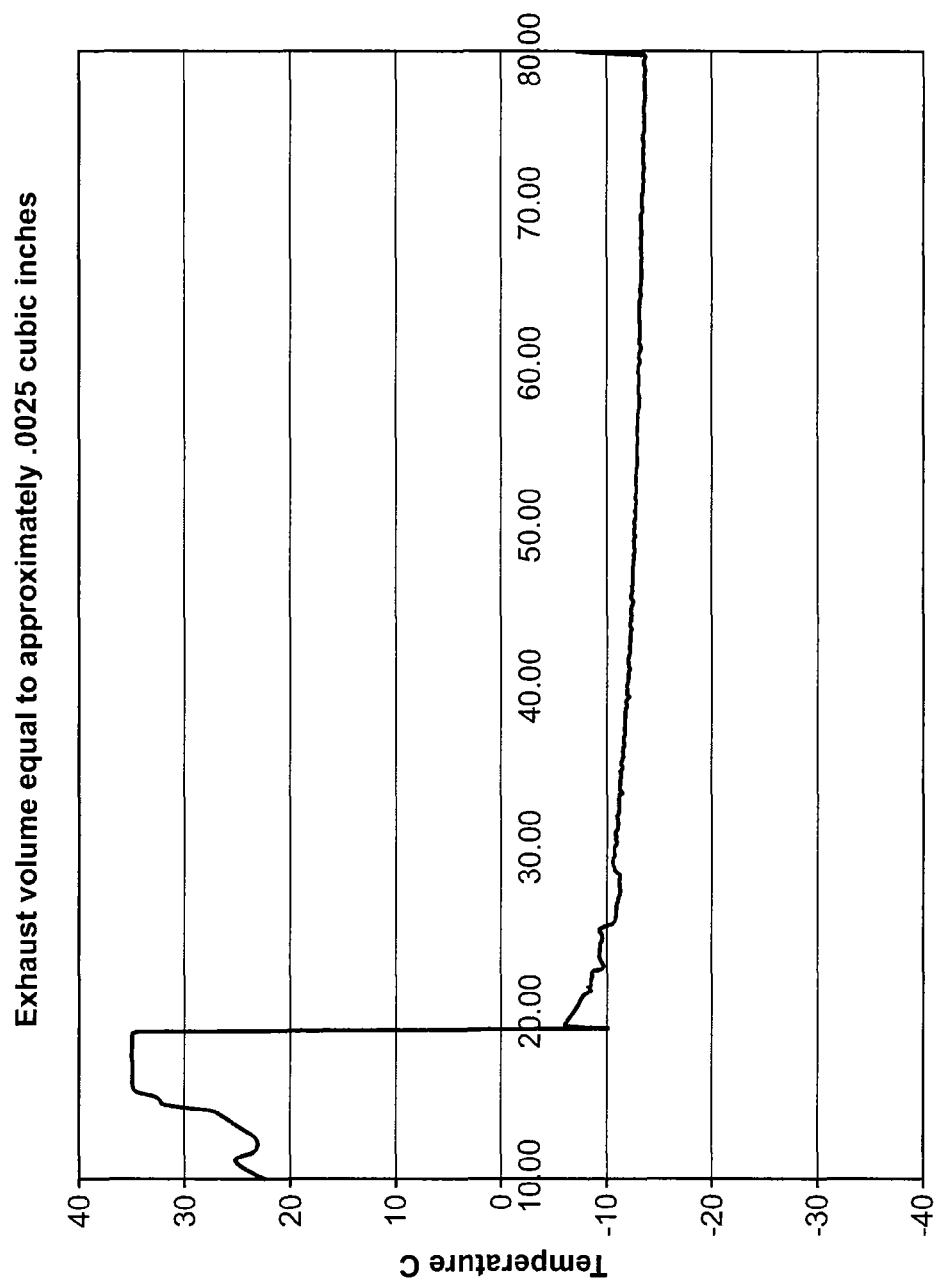


FIG. 13C

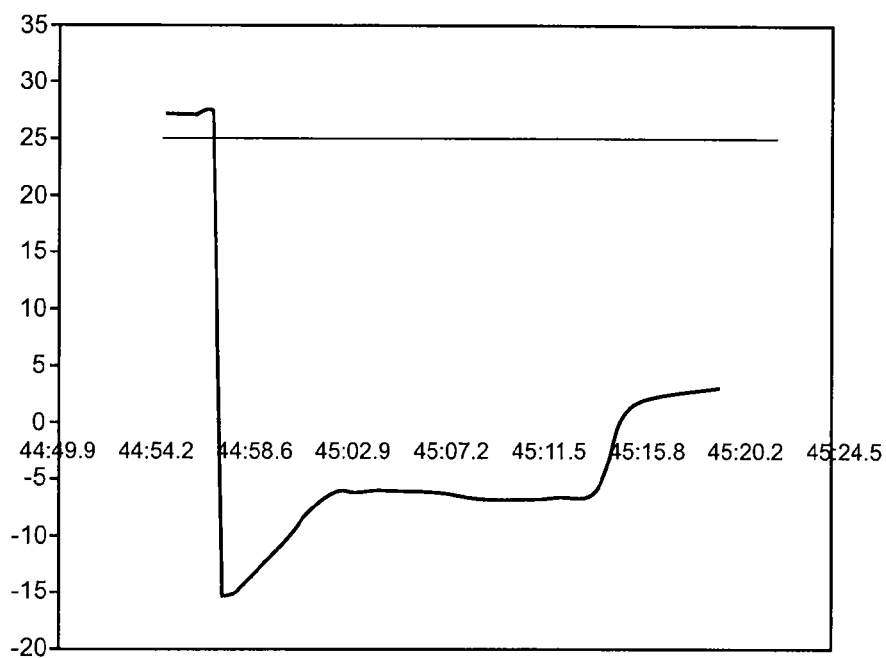


FIG. 13D

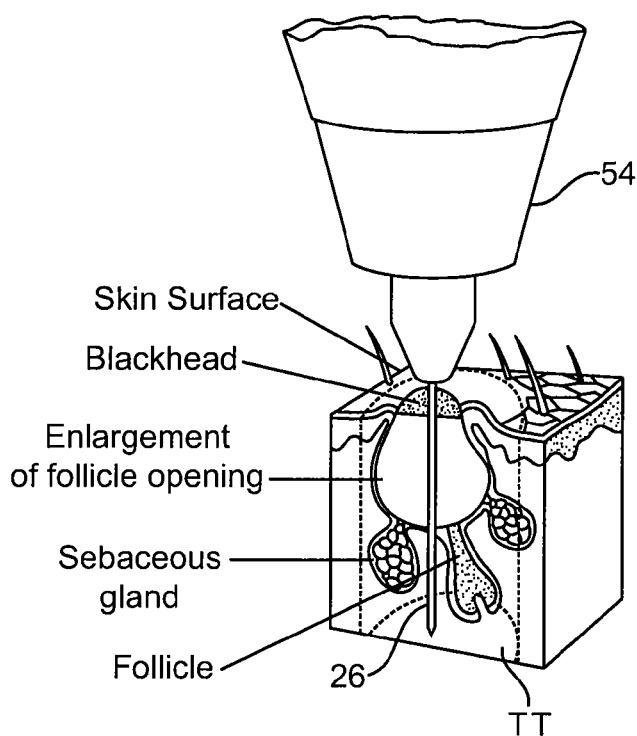


FIG. 14

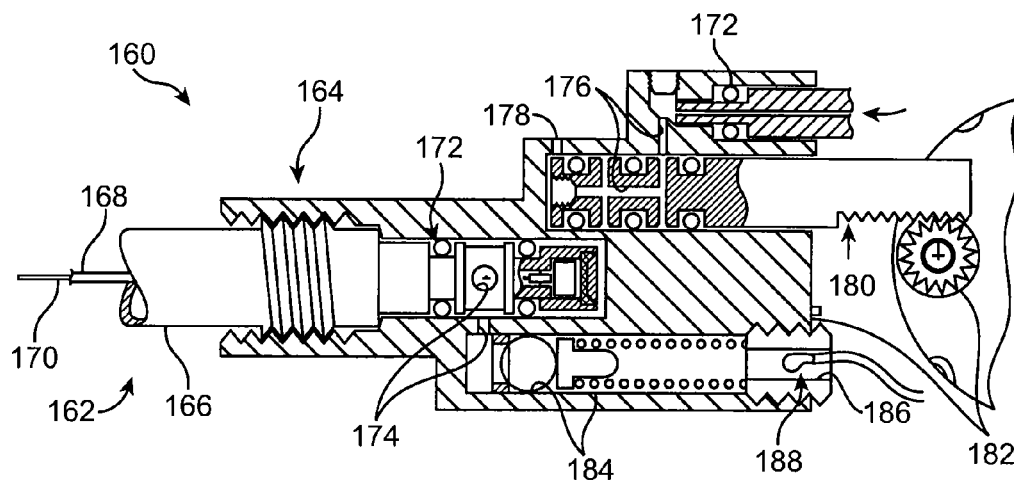


FIG. 16

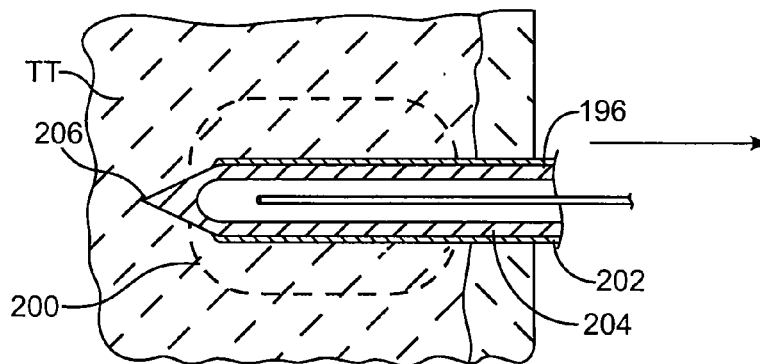


FIG. 17A

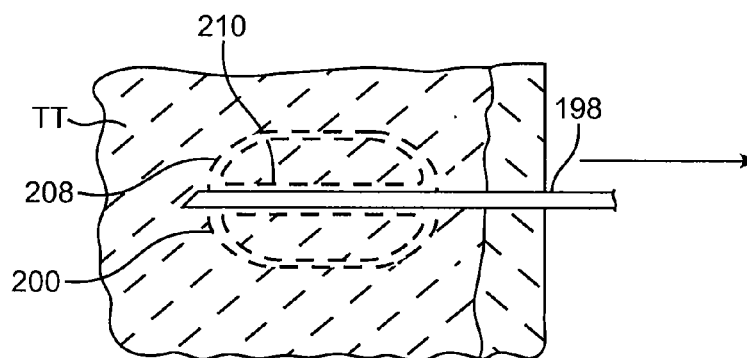


FIG. 17B

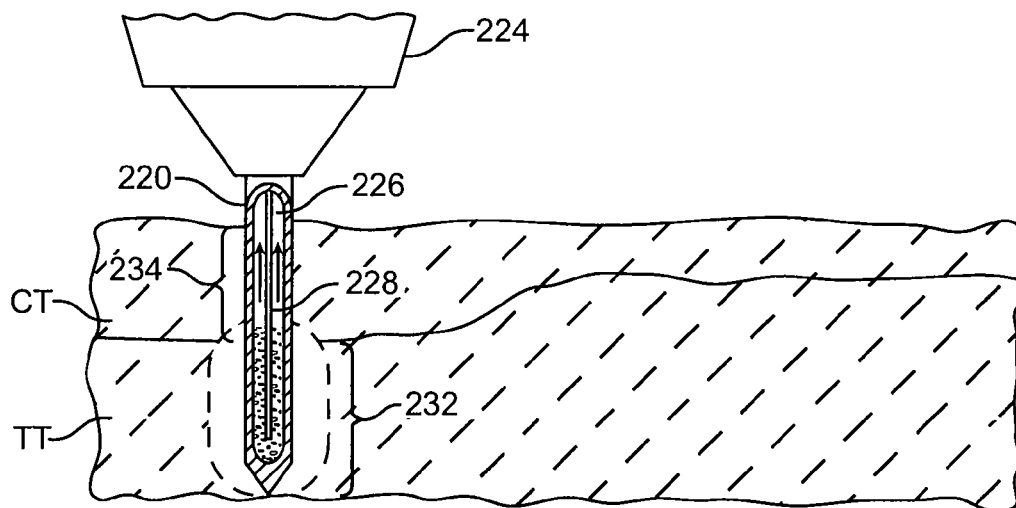


FIG. 18A

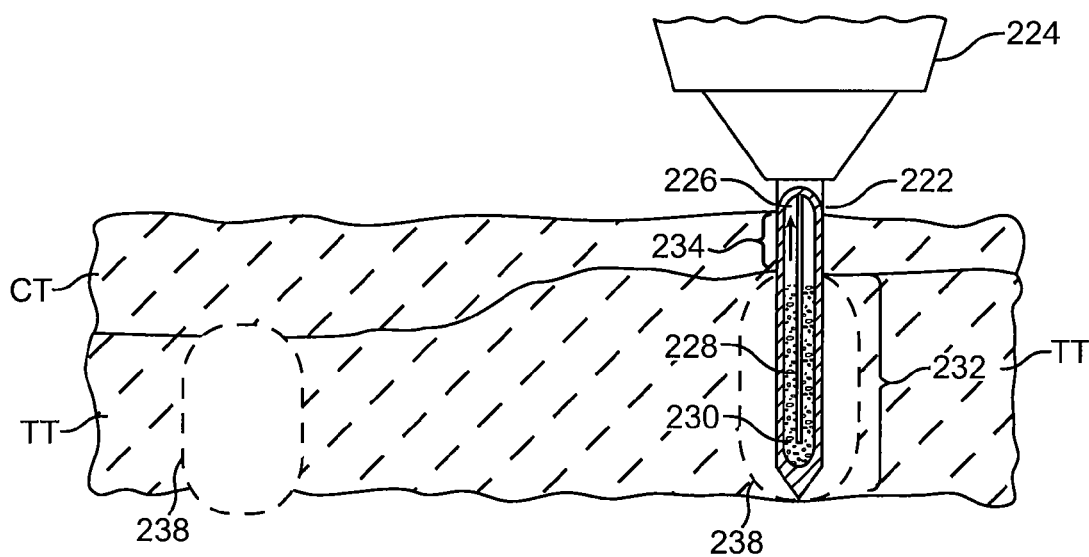


FIG. 18B

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**REPLACEABLE AND/OR EASILY
REMOVABLE NEEDLE SYSTEMS FOR
DERMAL AND TRANSDERMAL CRYOGENIC
REMODELING**

CROSS-REFERENCES TO RELATED
APPLICATIONS

This application is a continuation of U.S. patent application Ser. No. 11/675,886, filed Feb. 16, 2007, the entire content of which is incorporated herein by reference for all purposes.

STATEMENT AS TO RIGHTS TO INVENTIONS
MADE UNDER FEDERALLY SPONSORED
RESEARCH AND DEVELOPMENT

Not Applicable

REFERENCE TO A "SEQUENCE LISTING," A
TABLE, OR A COMPUTER PROGRAM LISTING
APPENDIX SUBMITTED ON A COMPACT DISK.

Not Applicable

BACKGROUND OF THE INVENTION

The present invention is generally directed to medical devices, systems, and methods, particularly for cooling-induced remodeling of tissues. Embodiments of the invention include devices, systems, and methods for applying cryogenic cooling to dermatological tissues so as to selectively remodel one or more target tissues along and/or below an exposed surface of the skin. Embodiments may be employed for a variety of cosmetic conditions, optionally by inhibiting undesirable and/or unsightly effects on the skin (such as lines, wrinkles, or cellulite dimples) or on other surrounding tissue. Other embodiments may find use for a wide range of medical indications. The remodeling of the target tissue may achieve a desired change in its behavior or composition.

The desire to reshape various features of the human body to either correct a deformity or merely to enhance one's appearance is common. This is evidenced by the growing volume of cosmetic surgery procedures that are performed annually.

Many procedures are intended to change the surface appearance of the skin by reducing lines and wrinkles. Some of these procedures involve injecting fillers or stimulating collagen production. More recently, pharmacologically based therapies for wrinkle alleviation and other cosmetic applications have gained in popularity.

Botulinum toxin type A (BOTOX®) is an example of a pharmacologically based therapy used for cosmetic applications. It is typically injected into the facial muscles to block muscle contraction, resulting in temporary enervation or paralysis of the muscle. Once the muscle is disabled, the movement contributing to the formation of the undesirable wrinkle is temporarily eliminated. Another example of pharmaceutical cosmetic treatment is mesotherapy, where a cocktail of homeopathic medication, vitamins, and/or drugs approved for other indications is injected into the skin to deliver healing or corrective treatment to a specific area of the body. Various cocktails are intended to effect body sculpting and cellulite reduction by dissolving adipose tissue, or skin resurfacing via collagen enhancement. Development of non-pharmacologically based cosmetic treatments also continues. For example, endermology is a mechanical based therapy that

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utilizes vacuum suction to stretch or loosen fibrous connective tissues which are implicated in the dimpled appearance of cellulite.

While BOTOX® and/or mesotherapies may temporarily reduce lines and wrinkles, reduce fat, or provide other cosmetic benefits they are not without their drawbacks, particularly the dangers associated with injection of a known toxic substance into a patient, the potential dangers of injecting unknown and/or untested cocktails, and the like. Additionally, while the effects of endermology are not known to be potentially dangerous, they are brief and only mildly effective.

In light of the above, it would be desirable to provide improved medical devices, systems, and methods, particularly for treatment of wrinkles, fat, cellulite, and other cosmetic defects. It would be particularly desirable if these new techniques provided an alternative visual appearance improvement mechanism which could replace and/or complement known bioactive and other cosmetic therapies, ideally allowing patients to decrease or eliminate the injection of toxins and harmful cocktails while providing similar or improved cosmetic results. It would also be desirable if such techniques were performed percutaneously using only local or no anesthetic with minimal or no cutting of the skin, no need for suturing or other closure methods, no extensive bandaging, and limited or no bruising or other factors contributing to extended recovery or patient "down time". It would further be desirable to provide new devices, systems, and methods for treatment of other cosmetic and/or dermatological conditions (and potentially other target tissues), particularly where the treatments may be provided with greater accuracy and control, less collateral tissue injury and/or pain, and greater ease of use.

BRIEF SUMMARY OF THE INVENTION

The present invention generally provides improved medical devices, systems, and methods. Embodiments may be particularly well suited for the treatment of dermatological and/or cosmetic defects, and alternative embodiments may be configured for treatment of a wide range of target tissues. Some embodiments of the present invention apply cooling with at least one small, tissue-penetrating probe, the probe often comprising a needle having a size suitable for inserting through an exposed surface of the skin of a patient without leaving a visible scar. The cooling may remodel one or more target tissue so as to effect a desired change in a composition of the target tissue and/or a change in its behavior. Unlike the large format cryogenic cooling systems of the past, small cryogenic cooling needle probes may dull or be damaged by insertion. Exemplary embodiments make use of replaceable needle probes supported by a probe body handle, with small needle probes often being replaced during treatment of a single patient. Careful control over the cryogenic cooling fluid introduced into a needle probe can allow the length of the active cooling to be controlled through depletion of evaporating cryogenic cooling liquid. Hence, even needles having similar external structures may provide differing lengths of effective remodeling along the needle axis. Surprisingly, small cryogenic cooling needles and/or other cryogenic cooling probes having a lubricious coating will allow safe removal of the probe from the treatment region while at least a portion of the tissue remains frozen, significantly decreasing the overall time for a procedure involving many insertion/freeze/removal cycles.

In a first aspect, the invention provides a method for treating tissue of a patient. The method comprises inserting a first

needle through a first insertion point and into a first target region of the tissue by manipulating handle. The handle supports the first needle via a needle interface. The first target region is cooled with the first needle and the first needle is removed from the patient. The first needle is replaced in the needle interface with a second needle. The second needle is inserted through the second insertion point and into a second target region of the tissue by manipulating the handle. The second target region is cooled with the second needle.

The second needle may optionally have size and/or cooling characteristics which are similar to those of the first needle. Such needle replacement may be particularly useful when using small needles that can become dull after a limited number of insertions into the patient. In other embodiments, the second needle may have size and/or cooling characteristics that differ from those of the first needle, such as having a different length, needle gauge size or diameter, active cooling length, or the like. In some embodiments, the first needle may be included in a first needle assembly that has only a single needle, while the second needle is included in a needle assembly having a plurality of needles. The needles of the second needle assembly may be simultaneously inserted into the target tissue, with the needles often being substantially parallel. A cooling fluid supply tube (and its associated lumen) may extend from a common cooling fluid supply of the needle interface, and cooling fluid vaporization lumens of each needle may flow to a common pressure-regulated exhaust path, also often via the needle interface. In many embodiments, cooling with the plurality of needles of the second needle assembly may be performed so that the cooled tissues are remodeled throughout a contiguous treatment zone. In other embodiments, the needle spacing and the like may result in a plurality of discrete remodeled zones.

Typically, the first and second needles will each have a sharpened distal tip and a 20-gauge needle size or less. The needles may be disposed of after use to avoid inserting a dull needle into the patient, with the needles optionally being inserted a single time, or alternatively being inserted a plurality of times (often less than ten times, and in many cases, less than five times) through the patient's skin. The handle of the system may be included in a probe body, and a fluid supply cartridge and battery may be supported and/or housed by the probe body. The probe body may be disposed of so that one or all of these components are used to treat only a single patient. Such a structure also helps avoid any requirement for a tether, power port, flexible supply line, or the like, which might otherwise inhibit manipulation and use of the hand-held probe. Cooling will often be terminated by closing a cooling fluid shutoff valve disposed along a cooling fluid supply path between a cooling fluid source and the lumen. As cooling may be performed by evaporating liquid cooling fluid within a lumen of the needle, a volume of the supply path between the valve and the lumen will preferably be quite low (typically being less than 0.05 cubic inches, optionally being less than 0.005 cubic inches) so as to allow more accurate control of the treatment time. The supply path between the valve and the needle lumen is preferably vented when the valve is closed so as to avoid continuing cooling by any residual cryogenic liquid within that volume.

In another aspect, the invention provides a method for treating a target tissue of a patient. The method comprises inserting a cooling probe distally through a collateral tissue and into the target tissue. The cooling probe has a lumen with a distal portion adjacent the target tissue and a proximal portion adjacent the collateral tissue. Cooling fluid is introduced into the distal portion of the lumen, and evaporation of liquid from the cooling fluid into gas occurs as the cooling

fluid flows proximally within the distal portion of the lumen. This evaporation occurs so that the evaporation cools the target tissue sufficiently for the desired remodeling treatment. Additionally, the evaporation occurs so that the liquid is depleted from the cooling fluid sufficiently when the gas passes through the proximal portion of the lumen to inhibit cooling of the collateral tissue.

The target tissue along the distal portion of the lumen can be cooled to a treatment temperature which is in a first temperature range. The collateral tissue along the proximal portion of the lumen will typically be cooled to a collateral tissue temperature in a second temperature range that is warmer than the first temperature range. Note that the differential in cooling effects between the distal and proximal lumen portions may occur despite the structure of the needle having a substantially uniform and/or consistent cross-section along the proximal and distal portions. Advantageously, a length of the distal, tissue remodeling portion may be selected from among a plurality of alternative lengths by selecting the probe for mounting to a probe body. Alternative probes may include differing cooling fluid supply paths so as to introduce differing cooling fluid supply flows with corresponding differing liquid depletion characteristics. More specifically, using otherwise similar probe structures having differing cooling fluid supply tubes with differing inner diameters and/or differing lengths may effectively vary the axial length of tissue that is remodeled, particularly where a significant portion of the metering of the cooling fluid flow is effected by the flow resistance of the cooling fluid supply lumen. Advantageously, the treatment temperatures along the distal portion may remain substantially uniform so long as there continues to be a sufficient mixture of cooling liquid and evaporated gas in the cooling fluid flow. As the cooling fluid liquid is depleted from that flow, temperatures of the flow may increase and/or the heat transfer from the surrounding probe structure (and tissue) may significantly decrease, with the change in cooling during a relatively short and predictable axial length of the probe.

In another aspect, the invention provides a method for remodeling a target tissue of a patient. The method comprises inserting a cooling probe distally into the target tissue. The target tissue is cooled sufficiently to freeze a region of the target tissue. The cooling probe is removed from the target tissue while the region remains frozen.

In many embodiments, the cooling probe may be removed less than 15 seconds after the termination of cooling, with the probe typically being removed less than 10 seconds after the cooling (or even less than 5 seconds after the cooling). Such counterintuitive removal of a cryogenic cooling probe from a still-frozen treatment region may be safely performed, for example, where the cooling is effected using a cooling probe having a cross-sectional size of a 20-gauge needle or less, the needle often being 25 gauge or less, and ideally being 30 gauge. A melted zone may be relatively quickly formed between such a probe and the surrounding frozen tissue to facilitate safe removal of the probe, despite the region remaining frozen. Hence, not all of the initially-frozen tissue may remain frozen during removal, although the majority of the tissue that has been frozen may remain frozen in many embodiments.

Many embodiments of the present invention may facilitate removal of a cryogenic treatment probe from a still-frozen tissue region by cooling the target tissue through a lubricious coating of the probe. Although the lubricious coating will often have a thermal conductivity which is significantly lower than that of the underlying probe material (the probe material typically comprising stainless steel hypotube or the like for

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small needle probes), the total thermal transfer from the target tissue can be facilitated by using a lubricious coating having a thickness which is significantly less than that of the probe material. Additionally, the internal temperature of a cryogenic fluid vaporization chamber or lumen may be selected to generate the desired cooling characteristics despite the thermal insulation of the lubricious coating. Nonetheless, overall treatment times will be significantly shorter, particularly where a large number of insertion/cooling/removal cycles are employed, and/or where the total cooling time is relatively short compared to the time for a total thaw of the frozen tissue.

In another aspect, the invention provides a system for treating tissue of a patient. The system comprises a first needle having a proximal end, a distal tissue-penetrating end, a lumen therebetween, and a cooling fluid supply lumen extending distally to a port within the needle lumen. The needle has a size of a 20-gauge needle or less. A second needle has a proximal end, a distal tissue-penetrating end and a lumen therebetween. A cooling fluid supply lumen extends distally to a port within the lumen of the second needle, the needle also having a size of a 20-gauge needle or less. A probe body has a handle supporting a cooling fluid source and a needle interface for sequentially receiving the first and second needles. Vaporization within the lumen of the received needle cools the tissue when the needle is inserted therein and cooling fluid is introduced from the cooling fluid supply through the port.

In another aspect, the invention provides a system for treatment of the target tissue of a patient. The patient has a collateral tissue adjacent the target tissue, and the system comprises a probe having a proximal end and a distal end. The distal end is insertable through the collateral tissue and into the target tissue. The inserted probe has a lumen with a proximal portion adjacent the target tissue and a distal portion adjacent the collateral tissue when the distal end is inserted. A cooling fluid source is in fluid communication with the distal portion of the lumen. The source is configured so that, when cooling fluid flows from the source into (and proximally along) the lumen of the inserted probe, liquid of the cooling fluid evaporates into gas within the distal portion of the lumen such that the evaporation cools the target tissue sufficiently for the treatment. Additionally, the liquid is depleted sufficiently when the cooling fluid passes through the proximal portion of the lumen to inhibit cooling of the collateral tissue.

In yet another aspect, the invention provides a system for remodeling a target tissue of the patient. The system comprises a cooling probe insertable distally into the target tissue. The cooling probe has a cooling surface for cooling the target tissue sufficiently to freeze a region of the target tissue. A lubricious coating is disposed over the cooling surface of the probe to facilitate removing the cooling probe from the target tissue while the region remains frozen.

Exemplary lubricious and/or hydrophobic coatings include polymers, such as a PTFE Teflon™ polymers, a silicone, or the like. Typical thicknesses of the coating may be from about 0.00005 inches to about 0.001 inches, with an exemplary PTFE polymer coating having a thickness of about 0.0005 inches and exemplary silicone coatings being thinner. In some embodiments, a portion of the probe (such as a distal end or small region near the distal end) may be free of the coating so as to allow use of the coating-free region as an electrode or the like.

BRIEF DESCRIPTION OF THE DRAWINGS

FIG. 1A is a perspective view of a self-contained subdermal cryogenic remodeling probe and system, according to an embodiment of the invention.

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FIG. 1B is a partially transparent perspective view of the self-contained probe of FIG. 1A, showing internal components of the cryogenic remodeling system and schematically illustrating replacement treatment needles for use with the disposable probe.

FIG. 2 schematically illustrates components that may be included in the treatment system.

FIG. 3 is a schematic cross-sectional view of an embodiment of a distal portion of the probe and system of FIG. 1B, showing a replaceable needle and an pressure relief valve with a limited exhaust volume.

FIG. 3A illustrates an exemplary fused silica cooling fluid supply tube for use in the replaceable needle of FIG. 3.

FIG. 4 is a more detailed view of a replaceable needle assembly for use in the system of FIGS. 1A and 1B.

FIGS. 5A-5C illustrate an exemplary supply valve for use in the probe and system of FIGS. 1A and 1B.

FIGS. 6-8 illustrate skin-engaging surfaces that selectably limit an effective insertable length of the needle, that apply pain-dulling pressure, and that apply inflammation-inhibiting cooling to the skin before and/or during treatment of the target tissue, respectively.

FIGS. 9, 9A, and 9B schematically illustrate a needle having an elongate cross-section to enhance the volume of treated tissue.

FIG. 10 schematically illustrates a thermal model of a cryogenic microprobe needle.

FIGS. 10A-10C graphically illustrate aspects of cryogenic cooling using nitrous oxide in the microprobe needles described herein.

FIGS. 11A and 11B schematically illustrate cross-sectional views cooling with a one needle system and a multiple needle system.

FIG. 12 graphically illustrates non-uniform cooling that can result from inadequate evaporation space within a small cryogenic needle probe.

FIGS. 13A-13D graphically illustrate effects of changes in exhaust volume on the cooling response by a small cryogenic needle probe.

FIG. 14 schematically illustrates a cryogenic microprobe needle system being used for a dermatological treatment.

FIG. 15 is a flow chart schematically illustrating a method for treatment using the disposable cryogenic probe and system of FIG. 1B.

FIG. 16 is a schematic cross-sectional view showing an alternative exemplary needle interface, along with the adjacent structures of the needle assembly and probe body.

FIGS. 17A and 17B are partial cross-sectional views schematically illustrating removal of a cryogenic cooling probe needle while at least a portion of the tissue remains frozen.

FIGS. 18A and 18B are partial cross-sectional views schematically illustrating how a depletion of liquid from a vaporizing cryogenic cooling fluid can be used to limit an effective treatment length on a portion of a cryogenic probe.

DETAILED DESCRIPTION OF THE INVENTION

The present invention provides improved medical devices, system, and methods. Embodiments of the invention will facilitate remodeling of tissues disposed at and below the skin, optionally to treat a cosmetic defect, a lesion, a disease state, and/or so as to alter a shape of the overlying skin surface.

Among the most immediate applications of the present invention may be the amelioration of lines and wrinkles, particularly by inhibiting muscular contractions which are associated with these cosmetic defects so as to improve an

appearance of the patient. Rather than relying entirely on a pharmacological toxin or the like to disable muscles so as to induce temporary paralysis, many embodiments of the invention will at least in part employ cold to immobilize muscles. Advantageously, nerves, muscles, and associated tissues may be temporarily immobilized using moderately cold temperatures of 10° C. to -5° C. without permanently disabling the tissue structures. Using an approach similar to that employed for identifying structures associated with atrial fibrillation, a needle probe or other treatment device can be used to identify a target tissue structure in a diagnostic mode with these moderate temperatures, and the same probe (or a different probe) can also be used to provide a longer term or permanent treatment, optionally by ablating the target tissue zone and/or inducing apoptosis at temperatures from about -5° C. to about -50° C. In some embodiments, apoptosis may be induced using treatment temperatures from about -1° C. to about -15° C., or from about -1° C. to about -19° C., optionally so as to provide a permanent treatment that limits or avoids inflammation and mobilization of skeletal muscle satellite repair cells. Hence, the duration of the treatment efficacy of such subdermal cryogenic treatments may be selected and controlled, with colder temperatures, longer treatment times, and/or larger volumes or selected patterns of target tissue determining the longevity of the treatment. Additional description of cryogenic cooling for treatment of cosmetic and other defects may be found in co-pending U.S. patent application Ser. No. 11/295,204, filed on Dec. 5, 2005 and entitled "Subdermal Cryogenic Remodeling of Muscle, Nerves, Connective Tissue, and/or Adipose Tissue (Fat)," the full disclosure of which is incorporated herein by reference.

In addition to cosmetic treatments of lines, wrinkles, and the like, embodiments of the invention may also find applications for treatments of subdermal adipose tissues, benign, pre-malignant lesions, malignant lesions, acne and a wide range of other dermatological conditions (including dermatological conditions for which cryogenic treatments have been proposed and additional dermatological conditions), and the like. Embodiments of the invention may also find applications for alleviation of pain, including those associated with muscle spasms. Hence, a variety of embodiments may be provided.

Referring now to FIGS. 1A and 1B, a system for cryogenic remodeling here comprises a self-contained probe handpiece generally having a proximal end 12 and a distal end 14. A handpiece body or housing 16 has a size and shape suitable for supporting in a hand of a surgeon or other system operator. As can be seen most clearly in FIG. 1B, a cryogenic cooling fluid supply 18 and electrical power source 20 are found within housing 16, along with a circuit 22 having a processor for controlling cooling applied by self-contained system 10 in response to actuation of an input 24. Some embodiments may, at least in part, be manually activated, such as through the use of a manual supply valve and/or the like, so that processors, electrical power supplies, and the like may be absent.

Extending distally from distal end 14 of housing 16 is a tissue-penetrating cryogenic cooling probe 26. Probe 26 is thermally coupled to a cooling fluid path extending from cooling fluid source 18, with the exemplary probe comprising a tubular body receiving at least a portion of the cooling fluid from the cooling fluid source therein. The exemplary probe 26 comprises a 30 g needle having a sharpened distal end that is axially sealed. Probe 26 may have an axial length between distal end 14 of housing 16 and the distal end of the needle of between about ½ mm and 5 cm, preferably having a length from about 1 cm to about 3 cm. Such needles may comprise a stainless steel tube with an inner diameter of about 0.006

inches and an outer diameter of about 0.012 inches, while alternative probes may comprise structures having outer diameters (or other lateral cross-sectional dimensions) from about 0.006 inches to about 0.100 inches. Generally, needle probe 26 will comprise a 16 g or smaller size needle, often comprising a 20 g needle or smaller, typically comprising a 25 g or smaller needle.

Addressing some of the components within housing 16, the exemplary cooling fluid supply 18 comprises a cartridge containing a liquid under pressure, with the liquid preferably having a boiling temperature of the less than 37° C. When the fluid is thermally coupled to the tissue-penetrating probe 26, and the probe is positioned within the patient so that an outer surface of the probe is adjacent to a target tissue, the heat from the target tissue evaporates at least a portion of the liquid and the enthalpy of vaporization cools the target tissue. A valve (not shown) may be disposed along the cooling fluid flow path between cartridge 18 and probe 26, or along the cooling fluid path after the probe so as to limit the temperature, time, rate of temperature change, or other cooling characteristics. The valve will often be powered electrically via power source 20, per the direction of processor 22, but may at least in part be manually powered. The exemplary power source 20 comprises a rechargeable or single-use battery.

The exemplary cooling fluid supply 18 comprises a single-use cartridge. Advantageously, the cartridge and cooling fluid therein may be stored and/or used at (or even above) room temperature. The cartridges may have a frangible seal or may be refillable, with the exemplary cartridge containing liquid N₂O. A variety of alternative cooling fluids might also be used, with exemplary cooling fluids including fluorocarbon refrigerants and/or carbon dioxide. The quantity of cooling fluid contained by cartridge 18 will typically be sufficient to treat at least a significant region of a patient, but will often be less than sufficient to treat two or more patients. An exemplary liquid N₂O cartridge might contain, for example, a quantity in a range from about 7 g to about 30 g of liquid.

Processor 22 will typically comprise a programmable electronic microprocessor embodying machine readable computer code or programming instructions for implementing one or more of the treatment methods described herein. The microprocessor will typically include or be coupled to a memory (such as a non-volatile memory, a flash memory, a read-only memory ("ROM"), a random access memory ("RAM"), or the like) storing the computer code and data to be used thereby, and/or a recording media (including a magnetic recording media such as a hard disk, a floppy disk, or the like; or an optical recording media such as a CD or DVD) may be provided. Suitable interface devices (such as digital-to-analog or analog-to-digital converters, or the like) and input/output devices (such as USB or serial I/O ports, wireless communication cards, graphical display cards, and the like) may also be provided. A wide variety of commercially available or specialized processor structures may be used in different embodiments, and suitable processors may make use of a wide variety of combinations of hardware and/or hardware/software combinations. For example, processor 22 may be integrated on a single processor board and may run a single program or may make use of a plurality of boards running a number of different program modules in a wide variety of alternative distributed data processing or code architectures.

Referring now to FIG. 2, the flow of cryogenic cooling fluid from fluid supply 18 is controlled by a supply valve 32. Supply valve may comprise an electrically actuated solenoid valve or the like operating in response to control signals from controller 22, and/or may comprise a manual valve. Exemplary supply valves may comprise structures suitable for

on/off valve operation, and may provide venting of the cooling fluid path downstream of the valve when cooling flow is halted so as to limit residual cryogenic fluid vaporization and cooling. More complex flow modulating valve structures might also be used in other embodiments.

The cooling fluid from valve 32 flows through a lumen 34 of a cooling fluid supply tube 36. Supply tube 36 is, at least in part, disposed within a lumen 38 of needle 26, with the supply tube extending distally from a proximal end 40 of the needle toward a distal end 42. The exemplary supply tube 36 comprises a fused silica tubular structure 36a having a polymer coating 36b (see FIG. 3A) and extends in cantilever into the needle lumen 38. Supply tube 36 may have an inner lumen with an effective inner diameter 36c of less than about 200 μm , the inner diameter often being less than about 100 μm , and typically being less than about 40 μm . Exemplary embodiments of supply tube 36 have inner lumens of between about 15 and 50 μm , such as about 30 μm . An outer diameter or size 36d of supply tube 36 will typically be less than about 1000 μm , often being less than about 800 μm , with exemplary embodiments being between about 60 and 150 μm , such as about 90 μm or 105 μm . The tolerance of the inner lumen diameter of supply tubing 36 will preferably be relatively tight, typically being about ± 10 μm or tighter, often being ± 5 μm or tighter, and ideally being ± 3 μm or tighter, as the small diameter supply tube may provide the majority of (or even substantially all of) the metering of the cooling fluid flow into needle 26.

Though supply tubes 36 having outer jackets of polyimide (or other suitable polymer materials) may bend within the surrounding needle lumen 38, the supply tube should have sufficient strength to avoid collapsing or excessive blow back during injection of cooling fluid into the needle. Polyimide coatings may also provide durability during assembly and use, and the fused silica/polymer structures can handle pressures of up to 100 kpsi. The relatively thin tubing wall and small outer size of the preferred supply tubes allows adequate space for vaporization of the nitrous oxide or other cooling fluid within the annular space between the supply tube 36 and surrounding needle lumen 38. Inadequate space for vaporization might otherwise cause a buildup of liquid in that annular space and inconsistent temperatures, as illustrated in FIG. 12. Exemplary structures for use as supply tube 36 may include the flexible fused silica capillary tubing sold commercially by Polymicro Technologies, LLC of Phoenix, Ariz. under model names TSP, TSG, and TSU, optionally including model numbers TSP 020090, TSPO40105, and/or others.

Referring now to FIGS. 2 and 3, the cooling fluid injected into lumen 38 of needle 26 will typically comprises liquid, though some gas may also be injected. At least some of the liquid vaporizes within needle 26, and the enthalpy of vaporization cools the tissue engaged by the needle. Controlling a pressure of the gas/liquid mixture within needle 26 substantially controls the temperature within lumen 38, and hence the treatment temperature range of the tissue. A relatively simple mechanical pressure relief valve 46 may be used to control the pressure within the lumen of the needle, with the exemplary valve comprising a valve body 48 (here in the form of a ball bearing) urged against a valve seat 50 by a biasing spring 52.

During initiation of a cooling cycle, a large volume along the cooling fluid pathway between the exit from the supply tube and exit from the pressure relief valve 46 may cause excessive transients. In particular, a large volume in this area may result in initial temperatures that are significantly colder than a target and/or steady state temperature, as can be seen in FIG. 13D. This can be problematic, particularly when (for example) the target temperature is only slightly warmer than

an undesirable effect inducing temperature, such as when remodeling through apoptosis or the like while seeking to inhibit necrosis. To limit such transients, the pressure relief valve 46 may be integrated into a housing 54 supporting needle 16, with the valve spring 52 being located outside the valve seat (and hence the pressure-control exit from pressure relief valve 46). Additionally, where needle 16 is included in a replaceable needle assembly 26A, pressure relief valve 46 is also located adjacent the interface between the needle assembly and probe handpiece housing 54. A detent 56 may be engaged by a spring supported catch to hold the needle assembly releasably in position, and the components of the needle assembly 26A (such as a brass or other metallic housing, a polyimide tubing 58, needle 16, and the like) may be affixed together using adhesive. Alternatively, as illustrated in FIGS. 1B and 4, the needle assembly and handpiece housing may have corresponding threads for mounting and replacement of the needle assembly. O-rings 60 can seal the cooling fluid pathway.

FIGS. 13A-13C present additional details on the effects of exhaust volume on cooling transients. In each case, a graph of temperature over time is shown for the outside temperature of an in vivo 30 g cooling needle with a target temperature of about -12°C . The devices were constructed with different exhaust volumes, with the volume being greater than about 0.009 in^3 in the embodiment of FIG. 13A. The embodiment of FIGS. 13B and 13C had exhaust volumes of about 0.009 in^3 and about 0.0025 in^3 , respectively. The data collection rate was about 0.7 sec for the embodiment of FIG. 13A, while the embodiments of FIGS. 13B and 13C both had data collection rates of about 0.1 sec, so that the actual nadir for the embodiment of FIG. 13A may have actually been significantly lower than that shown. Regardless, the exhaust volume is preferably less than about 0.05 in^3 , typically being less than 0.01 in^3 and/or 0.009 in^3 , and ideally being less than 0.005 in^3 .

Alternative methods to inhibit excessively low transient temperatures at the beginning of a refrigeration cycle might be employed instead of or together with the limiting of the exhaust volume. For example, the supply valve might be cycled on and off, typically by controller 22, with a timing sequence that would limit the cooling fluid flowing so that only vaporized gas reached the needle lumen (or a sufficiently limited amount of liquid to avoid excessive dropping of the needle lumen temperature). This cycling might be ended once the exhaust volume pressure was sufficient so that the refrigeration temperature would be within desired limits during steady state flow.

Additional aspects of the exemplary supply valves 32 can be understood with reference to FIGS. 2, 3, and 5A-5C. In FIG. 3, the valve is shown in the "on" configuration, with O-rings 60 sealing either side of the cooling fluid flow path and the cooling fluid flowing around the /movable valve member. In FIGS. 5A-5C, the cooling fluid flows through a passage 64 that extends axially along an alternative valve body of valve body 32' when the valve is in the on configuration (seen in FIG. 5B), with the O-rings being disposed between recesses in the movable valve body so as to allow the valve to operate when the valve body is in any rotational orientation about its axis. In both embodiments, the cooling fluid flow path downstream of the valve is vented when the valve is in the "off" configuration (in the embodiment of FIG. 3, by channel 66, and in the embodiment of FIGS. 5A-5C by the vaporizing cooling fluid flowing through the annular space between the valve body and the adjacent housing 54 so as to preserve the cooling fluid within the movable valve body).

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Venting of the cooling fluid from the cooling fluid supply tube **36** when the cooling fluid flow is halted by supply valve **32**, **32'** is advantageous to provide a rapid halt to the cooling of needle **16**. For example, a 2.5 cm long 30 g needle cooled to an outside temperature of -15°C . might use only about 0.003 g/sec of nitrous oxide after the system approaches or reaches steady state (for example, 10 seconds after initiation of cooling). If the total volume along the cooling fluid path from supply valve to the distal end or release port of supply tube **36** is about 0.1 cc, the minimum time to flow all the vaporizing liquid through the supply tube might be calculated as follows:

$$0.1 \text{ cc} \cdot (0.7 \text{ g/cc}) = 0.07 \text{ g of liquid nitrous oxide,}$$

$$0.07 \text{ g} / (0.003 \text{ g/sec}) = 23 \text{ sec.}$$

These calculation assume a fused silica supply tube sized to allow the minimum flow of nitrous oxide when fluid supply has a pressure of about 900 psi. When the supply valve is shut off, the pressure on the needle side of the supply valve would decay, causing the actual residual run time to be longer, with only a partial cooling near the distal tip of needle **16**. Regardless, it is desirable to limit the flow of cooling fluid into the needle to or near that which will vaporize in the needle so as to facilitate use of a simple disposable cooling fluid supply cartridge **18**. Analytical models that may be used to derive these cooling flows include that illustrated in FIG. **10**, which may be combined with the properties of the cooling fluid (such as the pressure/enthalpy diagram of nitrous oxide seen in FIG. **10A**) and the thermal properties of tissue shown in Table I to determine theoretical minimum cooling fluid flow rates (see FIG. **10B**), theoretical minimum cooling fluid quantities (see FIG. **10C**), and the like.

TABLE I

Property	Units	Value
Upper temperature bond of freezing (T_2)	$^{\circ}\text{C}$.	-1
Peak of phase transition temperature (T_3)	$^{\circ}\text{C}$.	-3
Lower Temperature bond of freezing (T_1)	$^{\circ}\text{C}$.	-8
Thermal conductivity in unfrozen region (k_u)	W/(mm- $^{\circ}\text{C}$.)	0.00063
Thermal conductivity in frozen region (k_f)	W/(mm- $^{\circ}\text{C}$.)	0.00151
Volumetric specific heat in unfrozen region ($\rho C_{p,u}$)	J/(mm 3 - $^{\circ}\text{C}$.)	0.00316
Volumetric specific heat in frozen region ($\rho C_{p,f}$)	J/mm 3 - $^{\circ}\text{C}$.	0.00193
Latent heat of solidification (HF)	J/mm 3	0.300

Referring now to FIGS. **3** and **4**, a wide variety of alternative embodiments and refinements may be provided. Fluid supply **18** may be initially opened for use by penetrating a frangible seal of the cartridge with a pierce point **70** (such as by tightening a threaded cartridge support coupled to housing **54**), with the nitrous being filtered by a filter **72** before being transmitted further along the cooling fluid path. Suitable filters may have pore sizes of from about 6 to about 25 μm , and may be available commercially from Porex of Georgia (or a variety of alternative suppliers), or may comprise a fine stainless steel screen (such as those having a mesh size of 635 with 0.0009" wire and spacing between the wire edges of approximately 0.0006"), or the like. A wide variety of epoxy or other adhesives **74** may be used, and the replaceable needle housing **24A** and other structural components may comprise a wide variety of metals or polymers, including brass or the like. Fins **76** may be included to help vaporize excess cooling liquid traveling proximally of the insertable length of needle **16**.

Very fine needles will typically be used to deliver to cooling at and/or below the surface of the skin. These needles can

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be damaged relatively easily if they strike a bone, or may otherwise be damaged or deformed before or during use. Fine needles well help inhibit damage to the skin during insertion, but may not be suitable for repeated insertion for treatment of numerous treatment sites or lesions of a particular patient, or for sequential treatment of a large area of the patient. Hence, the structures shown in FIGS. **1B**, **3**, and **4** allow the use probe bodies **16**, **54** with a plurality of sequentially replaceable needles. O-rings **60** help to isolate the cooling fluid supply flow (which may be at pressures of up to about 900 psi) from the exhaust gas (which may be at a controlled pressure in a range between about 50 and 400 psi, depending on the desired temperature). Exemplary O-rings may comprise hydrogenated Buna-N O-rings, or the like.

It may be advantageous to increase the volume of tissue treated by a single treatment cycle. As it is often desirable to avoid increasing the needle size excessively, along with selecting needles of different lengths, needle assemblies having differing numbers of needles in a needle array may also be selected and mounted to the probe body. Other embodiments may employ a single needle array fixedly mounted to the probe body, or a plurality of replaceable needle assemblies which all include the same number of needles. Regardless, cooling fluid flow to a plurality of needles may be provided, for example, by inserting and bonding a plurality of fused silica supply tubes into a 0.010 polyimide tubing **58** or header within the needle assembly, and by advancing the distal end of each supply tube into a lumen of an associated needle **16**. The needles might vent into a common exhaust space coaxially around polyimide tubing **58** in a manner similar to the single needle design shown. This can increase the quantity of tissue treated adjacent and/or between needles, as can be seen by comparing the theoretical 15 second exposures to one and two needles having a -15°C . probe surface, as shown in FIGS. **11A** and **11B**, respectively.

Referring now to FIG. **6**, it may be desirable to allow a system user to select a treatment depth, and/or to treat the skin surface to a temperature similar to that of the underlying target tissue along needle **16**. A distally oriented surface **82** supported by probe body **54** adjacent and/or around the proximal end of the needles may be configured to limit heat transfer to or from the skin when the needle **16** is inserted so that surface **82** engages the skin and cooling fluid flows into the needle. Exemplary heat transfer limiting surfaces may be formed, for example, from a small rigid foam pad or body **84**. Closed cell polyethylene foam or StyrofoamTM foam bodies may be used. As seen in FIG. **6**, an alternatively selectable set of bodies may also have differing thicknesses between the skin engaging-surface **82** and a surface **86** that engages the distal portion of the probe body. A user can then select an insertable length of the needle by selecting an appropriate probe body **84**, **84a**, **84b** and mounting the selected probe body onto the needles. Skin engaging surface **82** of bodies **84**, **84a**, and **84b** (or some other skin engaging surface adjacent the distal end of the needle) may be used to apply pressure to the skin, lesion, and/or target tissue during treatment. Alternative insertable length varying arrangements may also be provided, including those having threaded or other articulatable structures supporting the skin engaging surface **82** relative to the adjacent probe body **54** and the like.

Referring now to FIG. **7**, the application of pressure before, during, and/or after cooling may help dull or otherwise inhibit sharp pain. Such pain may otherwise result from the skin penetration, cooling, or thawing of the target and/or collateral tissues. It may also be beneficial to obscure the patient's view of the cooling needles, and/or to cover the needles when not in use so as to inhibit needle-stick injuries and potential disease

transmission. Toward that end, skin-engaging surface **82** may be supported by an articulatable support structure having a first configuration (shown in solid in FIG. 7) and a second configuration (shown dashed in FIG. 7). A simple spring mechanism may be used to apply a desired contact force between the skin-engaging surface **82** and the patient before insertion and during cooling. More sophisticated arrangements can also be employed in which the needle is driven distally and then proximally relative to the skin engaging surface appropriate times after sufficient pressure is applied to the patient, and the like.

Referring now to FIG. 8, still further alternative embodiments may be provided, in this case to apply different cooling temperatures to the patient, and/or to apply cooling to the skin surface and to a target tissue adjacent needle **16**. For example, in the case of acne it may be desirable to have two different cooling target temperatures, with cooling on the skin surface to inhibit inflammation (such as to about -10°C.), and (see FIG. 14) cooling of a target tissue TT cylinder around needle **16** sufficient to kill bacteria in the sebaceous gland and enlarged follicle opening (such as to about -20°C.). This dual temperature treatment may be particularly beneficial for severe forms of acne involving cysts or nodules. To provide cooling of tissue engaging surface **82**, that surface may be thermally coupled to a chamber **88**. Cooling fluid may be transmitted into chamber **88** by a port of a cooling fluid supply tube **36**, and the pressure of chamber **88** (and hence the temperature within the chamber) can optionally be controlled by a dedicated additional pressure relief valve **46a**. As the pressure within chamber **88** may differ from that within the needle, different treatment temperatures may be provided. The structures described herein can also be combined, for example, with the dual skin surface/needle temperature treatment structure of FIG. 8 being compatible with the replaceable needle systems of FIGS. 1B, 3, and/or 4. The dual skin surface/needle treatment systems and methods may also be compatible, for example, with the articulatable skin surface supports of FIG. 7 so as to apply cooled pressure to the skin prior to and/or during needle insertion using a flexible fluid supply tube or the like.

Still further alternatives may also be provided, including systems that generate a high rate of cooling to promote necrosis of malignant lesions or the like. High cooling rates limit osmotic effects in the target tissue. Slow cooling may tend to promote ice formation between cells rather than within cells due to the osmotic effect. While such slow cooling can be provided where necrosis is not desired (such as through the use of a proportion supply valve to modulate flow, a processor generated on/off cycle during initial cooling, or the like), the needle probes described herein will often be well suited to induce rapid cooling rates of the target tissue by vaporizing the cooling fluid in close thermal and spatial proximity to that target tissue. Hence, where necrosis of cells by intracellular ice formation is desired, cooling rates of about 25°C./sec or more, or even about 50°C./sec or more can be provided.

Referring now to FIGS. 9, 9A, and 9B, needles having circular cross-sectional shapes can often be used, but may not always provide the desired surface area for the cross-sectional area of the needle. Increased surface area may decrease the amount of time the needle is inserted to cool a volume of tissue to a temperature in a target range. Hence, a needle with an elongate outer cross-section such as elliptical needle **90** may be desirable. A distal cutting edge **92** at the distal tip may facilitate insertion and a circular cross-section **94** near the proximal end may limit cooling adjacent the skin, while cooling of the target tissue therebetween is enhanced by elliptical cross-section **96**.

Referring now to FIG. 15, a method **100** facilitates treating a patient using a cryogenic cooling system having a self-contained disposable handpiece and replaceable needles such as those of FIG. 1B. Method **100** generally begins with a determination **110** of the desired tissue remodeling and results, such as the alleviation of specific cosmetic wrinkles of the face, the inhibition of pain from a particular site, the alleviation of unsightly skin lesions or cosmetic defects from a region of the face, or the like. Appropriate target tissues for treatment are identified **112** (such as the subdermal muscles that induce the wrinkles, a tissue that transmits the pain signal, or the lesion-inducing infected tissues), allowing a target treatment depth, target treatment temperature profile, or the like to be determined **114**. An appropriate needle assembly can then be mounted **116** to the handpiece, with the needle assembly optionally having a needle length, skin surface cooling chamber, needle array, and/or other components suitable for treatment of the target tissues. Simpler systems may include only a single needle type, and/or a first needle assembly mounted to the handpiece.

As described above, pressure, cooling, or both may be applied **118** to the skin surface adjacent the needle insertion site before, during, and/or after insertion **120** and cryogenic cooling **122** of the needle and associated target tissue. The needle can then be retracted **124** from the target tissue. If the treatment is not complete **126** and the needle is not yet dull **128**, pressure and/or cooling can be applied to the next needle insertion location site **118**, and the additional target tissue treated. However, as small gauge needles may dull after being inserted only a few times into the skin, any needles that are dulled (or otherwise determined to be sufficiently used to warrant replacement, regardless of whether it is after a single insertion, 5 insertions, or the like) during the treatment may be replaced with a new needle **116** before the next application of pressure/cooling **118**, needle insertion **120**, and/or the like. Once the target tissues have been completely treated, or once the cooling supply cartridge included in the self-contained handpiece is depleted, the used handpiece and needles can be disposed of **130**.

A variety of target treatment temperatures, times, and cycles may be applied to differing target tissues to as to achieve the desired remodeling. For example, (as more fully described in patent application Ser. No. 11/295204, previously incorporated herein by reference) desired temperature ranges to temporarily and/or permanently disable muscle, as well as protect the skin and surrounding tissues, may be indicated by Table II as follows:

TABLE II

Temperature	Skin	Muscle/Fat
37° C.	baseline	baseline
25° C.	cold sensation	
18° C.	reflex vasodilation of deep blood vessels	
15° C.	cold pain sensation	
12° C.	reduction of spasticity	
10° C.	very cold sensation	
	reduction of chronic oedema	
	Hunting response	
5° C.	pain sensation	
0° C.	freezing point	
-1° C.		Phase transition begins
-2° C.		minimal apoptosis
-3° C.		Peak phase transition
-5° C.	tissue damage	moderate apoptosis
-8° C.		Completion of phase transition
-10° C.		considerable apoptosis

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TABLE II-continued

Temperature	Skin	Muscle/Fat
-15° C.		extensive apoptosis mild-moderate necrosis
-19° C.		apoptosis in some skeletal muscle tissues
-40° C.		extensive necrosis

To provide tissue remodeling with a desired or selected efficacy duration, tissue treatment temperatures may be employed per Table III as follows:

TABLE III

Cooled Temperature Range	Time Effectiveness	Purpose
≥0° C.	Treatment lasts only while the needle is inserted into the target tissue.	Can be used to identify target tissues.
From 0° C. to -5° C.	Often lasts days or weeks, and target tissue can repair itself. Embodiments may last hours or days.	Temporary treatment. Can be used to evaluate effectiveness of remodeling treatment on skin surface shape or the like.
From -5° C. to -15° C.	Often lasts months to years; and may be permanent. Limited muscle repair. Embodiments may last weeks to months.	Long term, potentially permanent cosmetic benefits. Can be deployed in limited doses over to time to achieve staged impact, controlling outcome and avoiding negative outcome. May be employed as the standard treatment.
From -15° C. to -25° C.	Often lasts weeks or months. Muscle may repair itself via satellite cell mobilization. Embodiments may last years.	May result in Mid-term cosmetic benefits, and can be used where permanent effects are not desired or to evaluate outcomes of potentially permanent dosing. Embodiments may provide permanent treatment.

There is a window of temperatures where apoptosis can be induced. An apoptotic effect may be temporary, long-term (lasting at least weeks, months, or years) or even permanent. While necrotic effects may be long term or even permanent, apoptosis may actually provide more long-lasting cosmetic benefits than necrosis. Apoptosis may exhibit a non-inflammatory cell death. Without inflammation, normal muscular healing processes may be inhibited. Following many muscular injuries (including many injuries involving necrosis), skeletal muscle satellite cells may be mobilized by inflammation. Without inflammation, such mobilization may be limited or avoided. Apoptotic cell death may reduce muscle mass and/or may interrupt the collagen and elastin connective chain. Temperature ranges that generate a mixture of these apoptosis and necrosis may also provide long-lasting or permanent benefits. For the reduction of adipose tissue, a permanent effect may be advantageous. Surprisingly, both apoptosis and necrosis may produce long-term or even permanent results in adipose tissues, since fat cells regenerate differently than muscle cells.

Referring now to FIG. 16, an exemplary interface 160 between a cryogenic cooling needle probe 162 and the associated probe body structure 164 are illustrated, along with adjacent portions of the needle, valve, probe body, and the like. Needle probe 162 is included in a needle assembly having a needle hub 166 with a lumen containing a polyimide tube 168 around a fused silica cooling fluid supply tube with its polyimide jacket 170. O-rings 172 seal in exhaust gas path 174 and inlet cooling fluid path 176, with the inlet path having a vent 178 to minimize run-on cooling when the cooling fluid

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supply is shut off by a valve 180, as generally described above. The valve is here actuated by a motor 182, while the exhaust gas pressure is controlled using a biasing spring and ball valve 184 as described above. A hollow set screw 186 can be used to assemble and/or adjust the pressure relief valve, and a thermistor 188 can be used to sense cooling gas flow.

Referring now to FIGS. 17A and 17B, cryogenic cooling probes 196, 198 are inserted into a target tissue TT and a flow of cryogenic cooling fluid is injected into the needle as generally described above. A region 200 of target tissue TT is cooled sufficiently to freeze and effect the desired remodeling of at least a portion of the target tissue. Rather than waiting for

the frozen target tissue to thaw, in the embodiment of FIG. 17A a lubricious coating 202 facilitates removal of the needle while at least a portion of the frozen target tissue remains frozen. The lubricious coating 202 may comprise a material having a thermal conductivity which is significantly less than that of the underlying probe structure 204. Coating 202 may have a thickness which is significantly less than that of the underlying probe structure 204, limiting the total insulation effect of the coating, and/or an interior temperature of probe 196 may be reduced so as to provide the desired overall cooling treatment. While it may be counterintuitive to cool the target tissue through a thermally insulating lubricious coating, the ability to more rapidly remove probe 196 from the patient can significantly increase the speed with which procedures may be performed, particularly when a large number of insertion/cooling/removal cycles are involved, and/or when the thaw time is at least half as long as (often being as long as or longer than) the active cooling time.

Note that a small surface 206 of probe 196 may be free of lubricious coating 202. Where the underlying probe structure 204 comprises an electrical conductor such as stainless steel or some alternative metal, the uncovered surface portion 206 may be used as an electrode for neurostimulation during positioning of probe 196 or the like.

In the embodiment of FIG. 17B, the use of cryosurgical probes of small diameter may facilitate removal of the probe without having to wait for a complete thaw of region 200. In this embodiment, microneedle probe 198 has a cross-sectional size of a 20-gauge needle or less, preferably comprising a 25-gauge needle or smaller, and ideally comprising a 30-gauge needle.

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These small diameter microneedle probes have little thermal mass and can be warmed relatively quickly by conduction from adjacent tissues and/or by any warm fluids flowing therein. As a result, while a major portion **208** of the target tissue remains frozen a layer **210** disposed between the still-frozen region and probe **198** may facilitate safe removal of the probe from the patient. Thawed layer **210** may comprise thawed target tissue, thawed extracellular fluids, or the like. Small needles also have small probe/tissue interface surface areas which may limit the total stiction between the probe and frozen tissue. Regardless of any particular mechanism of action, the use of small diameter cryogenic microneedles may allow safe removal of the probe from a treated tissue in a time which is significantly less than that associated with complete thaw of the iceball that has been formed. Exemplary embodiments using a lubricious coating and/or small diameter probe may allow the probe to be removed within about 10 seconds of the cooling, optionally allowing safe removal within about 5 seconds of cooling or even within about 3 seconds of cooling.

Referring now to FIGS. **18A** and **18B**, appropriate metering of the cooling fluid into a cryogenic cooling probe **220**, **222**, can be used to control the length of the probe that applies a therapeutic cooling. Probes **220**, **222** are replaceably supported by a probe body **224** via a needle receptacle or interface, as generally described above. Each probe includes a lumen **226** with a cooling fluid supply tube **228** extending to a distal port **230**. Through proper selection of the length of the cooling fluid supply tube **228** and/or an inner diameter of the lumen within the supply tube, the supply tube can be used to meter cooling fluid. More specifically, as noted above, cooling of the target tissue **TT** along a distal portion **232** of probe **228** is cooled by evaporation of the liquid included in the cryogenic cooling fluid. As shown in FIG. **18A**, cooling of a collateral tissue **CT** proximal of the target tissue **TT** may be limited by controlling the amount of cooling fluid flow so that the vaporizing liquid is depleted by the time the flow reaches a proximal portion **234** of the probe. In the embodiment of FIG. **18B**, a greater length of probe **222** is cooled by providing a relatively larger quantity of cooling fluid (and liquid) flowing from the supply tube **238** into lumen **226** via port **230**, so that liquid remains present for vaporization throughout a longer distal portion **232** of the probe. Note that the difference in lengths of the cooled portion **232** may be provided despite making use of an outer probe structure that is similar in cross section and/or overall length.

While the proximal portion **234** of probes **220**, **222** may be cooled somewhat (via conduction from the distal portion **232** of the probe, from the passage of gas vaporized from the gas of the cooling fluid, or the like), a temperature of collateral tissue **CT** may remain above the remodeling treatment temperature of a treatment zone **238** within the target tissue. Hence, the collateral tissue may avoid injury despite the absence of any additional insulation on the proximal portion of the probe. This also facilitates the use of differing treatment zones **238** at different locations for a particular patient through the selection of needle assemblies having appropriate cooling fluid supply paths with the desired differing cooling fluid flow characteristics.

While the exemplary embodiments have been described in some detail for clarity of understanding and by way of example, a number of modifications, changes, and adaptations may be implemented and/or will be obvious to those as skilled in the art. For example, one or more temperature feedback loops may be used to control the treatments, with the tissue temperature optionally being taken using a temperature sensing needle having a temperature sensor disposed

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adjacent an outer cooled skin engaging surface of the needle. Hence, the scope of the present invention is limited solely by the independent claims.

What is claimed is:

1. A method for treating tissue of a patient using a device, the device comprising a handle, a fluid supply cartridge with a frangible seal, and a needle interface for rigidly receiving a needle, the method comprising:
 - rigidly attaching a first needle to the needle interface of the device;
 - penetrating the frangible seal of the fluid supply cartridge of the device;
 - inserting the first needle through a first insertion point and into a first target region of the tissue by manipulating the handle;
 - cooling the first target region with the first needle and removing the first needle from the patient;
 - removing the first needle from the needle interface;
 - rigidly attaching a second needle to the needle interface;
 - inserting the second needle through a second insertion point and into a second target region of the tissue by manipulating the handle;
 - cooling the second target region with the second needle; and
- wherein the cooling of the first target region and second target region occur during a single treatment of the patient;
- wherein the first and second cooling steps comprise:
 - inserting the attached needle distally through a collateral tissue and into the target tissue, the inserted needle having an outer lumen and a distal portion adjacent the target tissue and a proximal portion adjacent the collateral tissue;
 - introducing cooling fluid into the distal portion of the outer lumen;
 - controlling the introduction of the cooling fluid into the distal portion of the outer lumen such that the cooling fluid evaporates into gas and cools the target tissue sufficiently for treatment and such that the fluid is depleted sufficiently when gas passes through the proximal portion of the outer lumen to inhibit treatment of the collateral tissue
- wherein the first needle and second needle each include a cooling fluid supply lumen extending distally to a port within the outer lumen, and wherein the cooling fluid is introduced into the distal portion of the outer lumen by metering the fluid out of the port of the cooling fluid supply lumen of the attached needle, the cooling fluid supply lumen having an inner diameter of less than 140 μm .
2. The method of claim 1, wherein the first needle and second needle have a 20 gauge needle size or smaller.
3. The method of claim 2, wherein at least one of the first needle and second needle have a 25 gauge needle size or smaller.
4. The method of claim 3, wherein at least one of the first needle and second needle have a 30 gauge needle size or smaller.
5. The method of claim 1, wherein the first needle and second needle are included in a first needle assembly and second needle assembly, respectively, and wherein the first needle assembly and second needle assembly include an engagement feature for fittingly mating with the needle interface of the device.
6. The method of claim 1, wherein at least one of the first needle and the second needle does not have a circular cross-sectional shape.

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7. The method of claim 1, wherein the device comprises a battery.

8. The method of claim 1, further comprising the steps of depleting the fluid supply cartridge and disposing the device so that the device and fluid supply cartridge are used to treat only the patient.

9. The method of claim 1, wherein the target tissue along the distal portion of the outer lumen is cooled to a treatment temperature in a first temperature range, and wherein the collateral tissue along the proximal portion of the outer lumen is cooled to a collateral tissue temperature in a second temperature range, the second temperature range being warmer than the first temperature range.

10. The method of claim 9, wherein the first temperature range is sufficient to freeze a portion of the target tissue.

11. A system for treating tissue of a patient, the system comprising:

a first needle having a proximal end, a distal tissue penetrating end, a lumen therebetween, and a cooling fluid supply lumen extending distally to a port within the lumen, the first needle having a 20 gauge needle size or smaller;

a second needle having a proximal end, a distal tissue penetrating end, a lumen therebetween, and a cooling fluid supply lumen extending distally to a port within the lumen, the second needle having a 20 gauge needle size or smaller;

a probe body having a handle supporting a cooling fluid source and a needle interface configured for sequentially receiving the first and second needles, the needle interface configured to rigidly attach a received needle such that the cooling fluid source is in communication with the cooling fluid supply lumen of a received needle;

wherein the cooling fluid source comprises a fluid supply cartridge and wherein the fluid supply cartridge comprises a frangible seal;

wherein the cooling fluid supply lumen of each of the first needle and the second needle meters fluid out of the port of the cooling fluid supply lumen, the cooling fluid supply lumen of each of the first needle and the second needle having an inner diameter of less than 140 μm .

12. The system of claim 11, wherein the second needle has a 25 gauge needle size or smaller.

13. The system of claim 12, wherein the second needle has a 30 gauge needle size or smaller.

14. The system of claim 11, wherein the first needle and second needle include an engagement feature on the proximal end for fittingly mating with the needle interface of the probe body.

15. The system of claim 14, wherein the engagement features of the first and second needles comprise a threaded engagement feature.

16. The system of claim 11, wherein the first needle and second needle have the same configuration.

17. The system of claim 11, wherein the first needle and second needle have a differing configuration.

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18. The system of claim 11, wherein the probe body comprises a pressure-regulated exhaust path configured to exhaust vaporized cooling fluid gas from the lumen of a received needle.

19. The system of claim 11, wherein the probe body further comprises a cooling fluid valve disposed along a cooling fluid supply path between the cooling fluid source and the lumen of a received needle, wherein opening of the valve induces cooling via evaporation of cooling fluid within the lumen of a received needle.

20. The system of claim 11, wherein the probe body further comprises a battery and a controller for controlling the cooling fluid flow from the cooling fluid source.

21. The system of claim 20, wherein the first needle and second needle are configured to be inserted into the patient such that a proximal portion of the needle is adjacent a collateral tissue and the distal end is adjacent the target tissue, and wherein the cooling fluid flow is controlled such that evaporation of the cooling fluid in the distal end of an attached needle treats the target tissue and such that the cooling fluid is depleted sufficiently when the cooling fluid passes through the proximal portion of an attached needle to inhibit treatment of the collateral tissue.

22. The system of claim 11, wherein the fluid supply cartridge is secured in a threaded cartridge support and wherein the frangible seal may be penetrated by the tightening of the threaded cartridge support.

23. A system for treating tissue of a patient, the system comprising:

a first needle having a proximal end, a distal tissue penetrating end, a lumen therebetween, and a cooling fluid supply lumen extending distally to a port within the lumen, the first needle having a 20 gauge needle size or smaller;

a second needle having a proximal end, a distal tissue penetrating end, a lumen therebetween, and a cooling fluid supply lumen extending distally to a port within the lumen, the second needle having a 20 gauge needle size or smaller;

a probe body having a handle supporting a cooling fluid source and a needle interface configured for sequentially receiving the first and second needles, the needle interface configured to rigidly attach a received needle such that the cooling fluid source is in communication with the cooling fluid supply lumen of a received needle;

wherein the cooling fluid source comprises a fluid supply cartridge and wherein the fluid supply cartridge contains a quantity in a range from 7 g to 30 g of liquid;

wherein the cooling fluid supply lumen of each of the first needle and the second needle meters fluid out of the port of the cooling fluid supply lumen, the cooling fluid supply lumen of each of the first needle and the second needle having an inner diameter of less than 140 μm .

* * * *